

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property
Organization
International Bureau



(43) International Publication Date
10 September 2004 (10.09.2004)

PCT

(10) International Publication Number
WO 2004/075787 A1

(51) International Patent Classification⁷: **A61F 2/01**

(21) International Application Number:
PCT/US2004/004096

(22) International Filing Date: 12 February 2004 (12.02.2004)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:
10/373,481 24 February 2003 (24.02.2003) US

(71) Applicant: SCIMED LIFE SYSTEMS INC. [US/US];
ONE SCIMED PLACE, MAPLE GROVE, MINNESOTA
55311 (US).

(72) Inventors; and

(75) Inventors/Applicants (for US only): BEULKE, MEL,
R. [US/US]; 7900 West 103Rd Street, Bloomington,
MN 55438 (US). BROOME, THOMAS, E. [US/US];
2465 Cambridge Way, Shakopee, MN 55438 (US). CAS-
SELL, ROBERT, L. [US/US]; 14398 -91st Street NE,
Otsego, MN 55330 (US). DANIEL, JOHN, M., K.
[US/US]; 359 Apache Court, Fremont, CA 94539 (US).
ESKURI, ALAN, D. [US/US]; 11650 Meadowbrook
Avenue, Hanover, MN 55341 (US). HANSEN, JAMES,
G. [US/US]; 12776 Verdin Street NW, Coon Rapids, MN
55448 (US). KOSTUR, GARY, R. [US/US]; 2119 Mar-
quis Road, Golden Valley, MN 55427 (US). MOLLAND,

DOUGLAS, B. [US/US]; 95 Sunrise Avenue, Tonka Bay,
MN 55331 (US). SMITH, SCOTT, R. [US/US]; 6950
County Road 10, Chaska, MN 55318 (US). VOGEL,
JEFFERY, H. [US/US]; 8243 Queen Avenue North,
Brooklyn Park, MN 55444 (US).

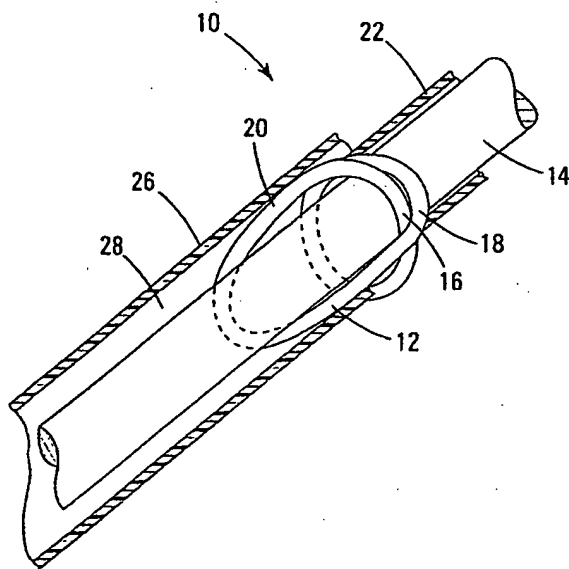
(74) Agent: SEAGER, Glenn, M.; Crompton Seager & Tufte
LLC, 1221 Nicollet Avenue, Suite 800, Minneapolis, MN
55403 (US).

(81) Designated States (unless otherwise indicated, for every
kind of national protection available): AE, AG, AL, AM,
AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN,
CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI,
GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE,
KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD,
MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG,
PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM,
TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM,
ZW.

(84) Designated States (unless otherwise indicated, for every
kind of regional protection available): ARIPO (BW, GH,
GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW),
Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), Euro-
pean (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR,
GB, GR, HU, IE, IT, LU, MC, NL, PT, RO, SE, SI, SK,
TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW,
ML, MR, NE, SN, TD, TG).

[Continued on next page]

(54) Title: APPARATUS FOR ANCHORING AN INTRAVASCULAR DEVICE ALONG A GUIDEWIRE



(57) Abstract: Anchoring mechanisms (e.g. 10, 110,
210, 310) for releasably securing an intravascular device
(114) along an elongated member such as a guidewire
(14) or catheter. The anchoring mechanism may include
an object that can be actuated between an unlocked
position and a locked position. In the unlocked position,
the anchoring mechanism is slidably and rotationally
disposed about the elongated member. In the locked
position, the anchoring mechanism is releasably secured
to the elongated member, preventing movement thereon.
A placement mechanism (e.g. 26, 126, 226, 326) such as
a tubular member can be utilized to actuate the anchoring
mechanism between the unlocked and locked positions.

WO 2004/075787 A1



Published:

- with international search report
- before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

APPARATUS FOR ANCHORING AN INTRAVASCULAR DEVICE ALONG A GUIDEWIRE

Field of the Invention

The present invention pertains to anchoring mechanisms for intravascular devices. More specifically, the present invention relates to anchoring mechanisms for releasably securing an intravascular device to an elongated member disposed within a blood vessel.

Background of the Invention

Medical procedures to treat occlusive vascular diseases, such as angioplasty, atherectomy and stent deployment, routinely involve the insertion and subsequent removal of various intravascular devices. In an angioplasty procedure, for example, a physician will typically advance a guidewire having an attached embolic protection filter to a desired location within the body, and subsequently deploy a balloon catheter to dislodge embolic debris or thrombus from a lesion. In some instances, the physician may wish to deploy more than one device during the procedure. For example, if the first embolic protection filter becomes occluded with debris dislodged during the angioplasty procedure, the physician may wish to replace the occluded filter with a second filter.

One limitation with the prior art is the inability to deploy more than one device along a single guidewire without having to remove the guidewire from the patient's body. Although more recent developments in the art have focused on the use of multiple wires to rapidly deploy and exchange such devices, techniques employing a single guidewire typically require the physician to remove the guidewire from the body prior to the insertion of another device.

Summary of the Invention

The present invention pertains to anchoring mechanisms for intravascular devices. More specifically, the present invention relates to anchoring mechanisms for releasably securing an intravascular device to a guidewire disposed within the vasculature of a patient.

In one exemplary embodiment of the present invention, an anchoring mechanism for releasably securing an intravascular device to a guidewire comprises an embolic protection filter actuatable between an unlocked (*i.e.* disengaged) position

and a locked (*i.e.* engaged) position. In the unlocked position, the anchoring mechanism is slidably and rotationally disposed along the guidewire, allowing the embolic protection filter to be advanced through the patient's vasculature. In the locked position, the anchoring mechanism is releasably secured to the guidewire, substantially preventing movement of the device along the guidewire. In certain implementations of the present invention, a placement device can be utilized to place the anchoring mechanism at a desired point along the guidewire. In other implementations, a retrieval mechanism can be utilized to disengage the anchoring mechanism from the guidewire.

Brief Description of the Drawings

Figure 1 is a cross-sectional view of an anchoring mechanism in accordance with an embodiment of the present invention, wherein the anchoring mechanism includes a spring coil;

Figure 2 is another cross-sectional view of the anchoring mechanism of Figure 1, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 3 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a split tube segment;

Figure 4 is another cross-sectional view of the anchoring mechanism of Figure 3, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 5 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes one or more leaf clamps;

Figure 6 is another cross-sectional view of the anchoring mechanism of Figure 5, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 7 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes one or more wires;

Figure 8 is another cross-sectional view of the anchoring mechanism of Figure 7, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 9 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a spring;

Figure 10 is another cross-sectional view of the anchoring mechanism of Figure 9, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 11 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a cam;

Figure 12 is another cross-sectional view of the anchoring mechanism of Figure 11, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 13 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention employing a cam;

Figure 14 is another cross-sectional view of the anchoring mechanism of Figure 13, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 15 is yet another cross-sectional view of the anchoring mechanism of Figure 13, wherein a decoupling tube is utilized to disengage the anchoring mechanism from the guidewire;

Figure 16 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes an elastomeric object;

Figure 17 is another cross-sectional view of the anchoring mechanism of Figure 16, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 18 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a shape-memory tube;

Figure 19 is another cross-sectional view of the anchoring mechanism of Figure 18, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 20 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes an expandable balloon;

Figure 21 is another cross-sectional view of the anchoring mechanism of Figure 20, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 22 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes an O-ring;

Figure 23 is another cross-sectional view of the anchoring mechanism of Figure 22, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 24 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes one or more deflectable tabs;

Figure 25 is another cross-sectional view of the anchoring mechanism of Figure 24, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 26 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a circular object;

Figure 27 is another cross-sectional view of the anchoring mechanism of Figure 26, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 28 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a flared collet;

Figure 29 is another cross-sectional view of the anchoring mechanism of Figure 28, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 30 is another cross-sectional view of the anchoring mechanism of Figure 28, wherein the anchoring mechanism further includes threads;

Figure 31 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes an offset block;

Figure 32 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a split-jawed collet and a spring;

Figure 33 is another cross-sectional view of the anchoring mechanism of Figure 32, wherein a retrieval sheath is secured to the anchoring mechanism;

Figure 34 is another cross-sectional view of the anchoring mechanism of Figure 32, wherein a second sheath and decoupling tube are utilized to disengage the anchoring mechanism from the guidewire;

Figure 35 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a sleeve;

Figure 36 is another cross-sectional view of the anchoring mechanism of Figure 35, wherein a retrieval sheath is secured to the anchoring mechanism;

Figure 37 is another cross-sectional view of the anchoring mechanism of Figure 35, wherein a second sheath and decoupling tube are utilizing to disengage the anchoring mechanism from the guidewire;

Figure 38 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes one or more latches;

Figure 39 is another cross-sectional view of the anchoring mechanism of Figure 38, wherein a retrieval sheath is secured to the anchoring mechanism;

Figure 40 is another cross-sectional view of the anchoring mechanism of Figure 35, wherein a second sheath is advanced along the guidewire;

Figure 41 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a wedge;

Figure 42 is another cross-sectional view of the anchoring mechanism of Figure 41, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 43 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention employing a wedge;

Figure 44 is another cross-sectional view of the anchoring mechanism of Figure 43, wherein the object is advanced along the wedge in a second position;

Figure 45 is yet another cross-sectional view of the anchoring mechanism of Figure 43, wherein anchoring mechanism is releasably secured to the guidewire in a third position;

Figure 46 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention employing a threaded wedge;

Figure 47 is another cross-sectional view of the anchoring mechanism of Figure 46, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 48 is a perspective view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a slotted tube;

Figure 49 is a cross-sectional view of the anchoring mechanism of Figure 48 along line 49-49;

Figure 50 is another perspective view of the anchoring mechanism of Figure 48, wherein the anchoring mechanism is shown slidably disposed along a guidewire after heat setting;

Figure 51 is another perspective view of the anchoring mechanism of Figure 48, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 52 is a perspective view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a slotted tube having multiple necked-down regions;

Figure 53 is a cross-sectional view of the anchoring mechanism of Figure 52 along line 53-53, showing the first necked-down portion;

Figure 54 is a cross-sectional view of the anchoring mechanism of Figure 52 along line 54-54, showing the second necked-down portion;

Figure 55 is another perspective view of the anchoring mechanism of Figure 52, wherein the anchoring mechanism is slidably disposed along the guidewire;

Figure 56 is another perspective view of the anchoring mechanism of Figure 52, wherein the anchoring mechanism is releasably secured to the guidewire;

Figure 57 is a cross-sectional view of an anchoring mechanism in accordance with another embodiment of the present invention, wherein the anchoring mechanism includes a slotted tube having a wall with varying section moduli;

Figure 58 is another cross-sectional view of the anchoring mechanism of Figure 57 along line 58-58, wherein the anchoring mechanism is slidably disposed along the guidewire; and

Figure 59 is another cross-sectional view of the anchoring mechanism of Figure 57, wherein the anchoring mechanism is releasably secured to the guidewire.

Detailed Description of the Invention

The following description should be read with reference to the drawings wherein like reference numerals indicate like elements throughout the several views. The detailed description and drawings illustrate example embodiments of the claimed invention. The drawings, which are not necessarily to scale, depict several embodiments and are not intended to limit the scope of the invention. Although examples of construction, dimensions, materials and manufacturing processes are illustrated for the various elements, those skilled in the art will recognize that many of the examples provided have suitable alternatives that may be utilized.

Figure 1 is a cross-sectional view illustrating an anchoring mechanism 10 in accordance with an exemplary embodiment of the present invention. Anchoring mechanism 10 comprises a spring coil 12 slidably and rotationally disposable about a

guidewire 14 in an unlocked (*i.e.* disengaged) position, and releasably securable to the guidewire 14 in a locked (*i.e.* engaged) position.

Spring coil 12 comprises a wire coil segment 16 adapted to receive guidewire 14, a distal portion 18, and a proximal portion 20. The distal portion 18 of spring coil 12 is attached to a proximal end 22 of an intravascular device such as an embolic protection filter (not shown). The proximal portion 20 of spring coil 12 extends proximally in a U shape such that when unconstrained radially, the proximal portion 20 of spring coil 12 expands radially, causing the wire coil segment 16 to contract and frictionally engage the guidewire 14.

In certain embodiments, spring coil 12 may be formed as a separate component, and then attached to the intravascular device proximal end 22 prior to insertion in the patient. Attachment of the spring coil 12 to the intravascular device proximal end 22 may be accomplished by any number of suitable attachment means, including soldering, welding, crimping and/or adhesive bonding. In other embodiments, the spring coil 12 and intravascular device may be formed as a single member using, for example, a mold injection process.

Spring coil 12 may be formed of any number of suitable materials biocompatible with the body. For example, spring coil 12 may be formed of a metal such as 303 or 316 stainless steel. Alternatively, the spring coil 12 may be formed of a polymeric material such as polypropylene (PP), polyvinyl chloride (PVC), polyethylene and/or polytetrafluoroethylene (PTFE). In one particular implementation, spring coil 12 may comprise a shape-memory material such as nickel-titanium alloy (Nitinol).

A placement tube 26 can be used to advance the anchoring mechanism 10 to a desired location within a blood vessel, and to actuate the spring coil 12 between the locked and unlocked positions. Placement tube 26 has an inner lumen 28 configured to disengage spring coil 12 from the guidewire 14 when disposed about the proximal portion 20. As shown in Figure 1, placement tube 26 can be used to compress the proximal portion 20 of spring coil 12 inwardly towards the guidewire 14, causing the wire coil segment 16 to expand slightly to permit the spring coil 12 to slide and rotate about the guidewire 14.

To engage the anchoring mechanism 10 along the guidewire 14, placement tube 26 is withdrawn proximally until the proximal portion 20 of spring coil 12 is unconstrained within the inner lumen 28, as shown in Figure 2. Once unconstrained

by the placement tube 26, the proximal portion 20 of spring coil 12 expands radially, causing the wire coil segment 16 to compress about the guidewire 14.

To release the anchoring mechanism 10 from the guidewire 14, placement tube 26 can be advanced distally along guidewire 14 until the proximal portion 20 is contained at least in part within inner lumen 28. Continued advancement of the placement tube 26 distally compresses the proximal portion 20, forcing the wire coil segment 16 to expand outwardly and disengage from the guidewire 14. Once disengaged from the guidewire 14, the anchoring mechanism 10 and attached intravascular device can then be withdrawn from the patient's body.

Figure 3 illustrates an anchoring mechanism 110 in accordance with another exemplary embodiment of the present invention. Anchoring mechanism 110 comprises a split tube segment 112 having a proximal section 134, a distal section 136, and a bend region 138. The distal section 136 of split tube segment 112 is biased to deflect inwardly to frictionally engage the guidewire 14.

A placement tube 126 can be utilized to advance the split tube segment 112 along the guidewire 14, and to actuate the distal section 136 between the unlocked and locked positions. Placement tube 126 has a proximal portion (not shown) and a distal portion 130. The distal portion 130 of placement tube 126 includes a reduced outer diameter portion 132 having an outer diameter that is smaller than the inner diameter of split tube segment 112, allowing the split tube segment 112 to slide thereon, thereby preventing the distal section 136 of split tube segment 112 from frictionally engaging the guidewire 14.

To frictionally engage the anchoring mechanism 110 about the guidewire, placement tube 126 is retracted proximally along the guidewire 14, permitting the distal section 136 of the split tube segment 112 to deflect inwardly and compress against the guidewire 14, as shown in Figure 4. To disengage the anchoring mechanism 110 from the guidewire 14, placement tube 126 can be advanced distally, forcing the distal section 136 of split tube segment 112 to disengage from the guidewire 14.

In the exemplary embodiment illustrated in Figures 3-4, split tube segment 112 is configured to function as a proximal stop for embolic protection filter 114, preventing movement of the filter 114 proximally thereof. As with any of the embodiments described herein, however, the split tube segment 112 may be attached to, or form part of, an embolic protection filter 114. In such cases, the anchoring

mechanism may be utilized to releasably secure the embolic protection filter 114 directly to the guidewire 14.

In another exemplary embodiment illustrated in Figure 5, an anchoring mechanism 210 in accordance with the present invention may include one or more leaf clamps. Anchoring mechanism 210 comprises a tube segment 212 having a proximal section 234, a distal section 236, and a bend region 238. The distal section 236 of tube segment 212 is biased to bend inwardly towards the guidewire 14, forming one or more leaf clamps adapted to frictionally engage the guidewire 14 in a locked position.

A placement tube 226 can be utilized to advance the tube segment 212 along the guidewire 14, and to actuate the distal section 236 between the unlocked and locked positions. Placement tube 226 has a distal section 230 having an outer diameter that is smaller than the inner diameter of the tube segment 212, allowing the distal section 230 of placement tube 226 to slide within tube segment 212. When placement tube 226 is inserted within tube segment 212 distal the bend region 238, the distal section 236 of tube segment 212 is substantially prevented from engaging the guidewire 14, as shown in Figure 5.

To engage the anchoring mechanism 210 along the guidewire 14, placement tube 226 is retracted proximally until the distal section 230 of the placement tube 226 is proximal bend region 238, permitting the distal section 236 of the tube segment 212 to deflect inwardly and compress against the guidewire 14, as shown in Figure 6. To subsequently release the lock, placement tube 226 can be advanced distally, forcing the distal section 236 of tube segment 112 to disengage from the guidewire 14.

Figure 7 illustrates an anchoring mechanism 310 in accordance with another exemplary embodiment of the present invention. Anchoring mechanism 310 comprises a tubular member 326 and one or more wires 312 adapted to frictionally engage the guidewire 14 in a locked position. Tubular member 326 has a proximal end (not shown) and a distal end 330. Each wire 312 is attached at a distal end 318 to the proximal end 322 of an intravascular device (e.g. an embolic protection filter). The proximal end 320 each wire 312, in turn, is attached to the distal end 330 of the tubular member 326.

To engage the anchoring mechanism 310 along the guidewire 14, tubular member 326 is rotated in either a clockwise or counterclockwise direction until the one or more wires 312 frictionally engage the guidewire 14, as shown in Figure 8. If

desired, an optional coating can be applied to the wires 312 and/or the guidewire 14 to increase the frictional force therebetween.

To subsequently release the anchoring mechanism 310 from the guidewire 14, placement tube 326 can be rotated in an opposite direction until the one or more wires 312 disengage from the guidewire 14. Once disengaged, the anchoring mechanism 310 and intravascular device can then be removed from the patient's body.

In a similar embodiment illustrated in Figure 9, an anchoring mechanism 410 in accordance with an exemplary embodiment of the present invention may include a tubular member 426 and a spring 412. Spring 412 is formed of a flexible wire having a distal end 418 and a proximal end 420. The distal end 418 of spring 412 is attached to the proximal portion 422 of an embolic protection filter. The proximal end 420 of spring 412, in turn, is attached the distal end 430 of tubular member 426.

In an unlocked position illustrated in Figure 9, spring 412 is adapted to slide and rotate about guidewire 14, allowing the intravascular device to be advanced along the guidewire 14 and placed at a desired location within the body. To engage the spring 412 along the guidewire 14, tubular member 426 is withdrawn proximally, forcing the spring 412 to stretch axially and compress radially about the guidewire 14. As with the previous embodiment, an optional coating can be applied to increase the frictional force between the guidewire 14 and the spring 412.

In another exemplary embodiment illustrated in Figure 11, an anchoring mechanism 510 in accordance with the present invention may employ a cam. Anchoring mechanism 510 comprises a tube segment 540 coupled to a proximal portion 522 of an embolic protection filter (not shown). Tube segment 540 includes an expanded portion 542 defining an inner chamber 544 having an inner wall surface 546.

Disposed within inner chamber 544 is an object 512 having a distal section 518 and a proximal section 520. The distal and/or proximal sections 518, 520 may each include a notch that permits the object ends 518, 520 to bend inwardly when compressed radially against the inner wall surface 546 of inner chamber 544.

In a first (*i.e.* unlocked) position illustrated in Figure 11, the object 512 is positioned within chamber 544 such that neither the proximal end 520 nor the distal end 518 of object 512 is in contact with the inner wall surface 546. In this position, the object 512 is slidably and rotationally disposed along the guidewire 14, allowing the intravascular device to be placed within the patient's vasculature.

To engage the anchoring mechanism 510 along the guidewire 14, the tube segment 540 and attached intravascular device can be moved along the guidewire 14, forcing the object 512 disposed within the chamber 544 to compress against the inner wall surface 546. Continued advancement of the tube segment 540 along the guidewire 14 forces one of the notched ends (e.g. proximal end 520) to bend inwardly and frictionally engage the guidewire 14, as shown in Figure 12.

Although the exemplary embodiment illustrated in Figures 11-12 shows an object having a notch formed on or both ends, it is contemplated that other objects can be utilized without deviating from the scope of the invention. In certain embodiments, for example, the object may comprise a ball, wedge or coil. In other embodiments, the geometry of the inner wall surface may be circular, rectangular or have an irregular shaped surface.

In one such variation illustrated in Figures 13-15, an anchoring mechanism 610 in accordance with an exemplary embodiment of the present invention comprises a circular object 612 disposed within a chamber 644 having an irregularly shaped inner wall surface 646. The inner wall surface 646 of tube segment 642 includes one or more recesses 648 substantially conforming in size and shape to the dimensions of the circular object 612.

In an first (*i.e.* unlocked), the circular object 612 is positioned within the inner chamber 644 such that the object 612 is not in contact with either of the recesses 648. To engage the anchoring mechanism 610 along the guidewire 14, tube segment 640 is moved along the guidewire 14 until the circular object 612 locks into one of the recesses 648, as shown in Figure 14.

To disengage the anchoring mechanism 610 from the guidewire 14, a decoupling tube 650 can be advanced along the guidewire 14 to disengage the circular object 612 from the recessed surface 648, as shown in Figure 15. The distal end 652 of the decoupling tube 650 may have a geometry corresponding in size and shape to the particular object employed. For example, the distal end 652 of decoupling tube 650 may be curved slightly to correspond with the shape of the circular object 612.

Figure 16 illustrates an anchoring mechanism 710 in accordance with another exemplary embodiment of the present invention. An elastomeric object 712 is coupled to a reduced inner diameter portion 722 disposed on the proximal end 722 of an embolic protection filter (not shown). The elastomeric object 712 is attached at a distal end 736 to the reduced inner diameter portion 722 at notch 754, and at a

proximal end 734 to a placement tube 726. In use, the elastomeric object 712 is configured to lock onto the guidewire 14 when unconstrained by a tab disposed on the distal end 730 of the placement tube 726.

In a first (*i.e.* unlocked) position illustrated in Figure 16, placement tube 726 is configured to attach to a proximal end 734 of the elastomeric object 712, causing it to stretch axially and disengage from the guidewire 14. To engage the anchoring mechanism 710 along the guidewire 14, placement tube 726 is retracted proximally, causing the proximal end 734 of the elastomeric object 712 to detach from the tab on the distal end 730 of the placement tube 726. Once detached, the elastomeric object 712 reverts to its natural, pre-stretched state, causing it to frictionally engage the guidewire 14, as shown in Figure 17.

Figure 18 illustrates an anchoring mechanism 810 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 810 comprises a shape memory tube 812 having a pre-defined shape which, when compressed radially by a placement tube 826, functions in an unlocked position, and when unconstrained radially, functions in a locked position. To bias the shape memory tube 812 to radially expand and frictionally engage the guidewire 14 in the locked position, a super elastic material such as a nickel titanium alloy (Nitinol) may be used.

In the exemplary embodiment illustrated in Figure 18, the distal end 818 of shape memory tube 812 further includes a joint 856 adapted to permit rotation of the shape memory tube 812 relative to the proximal end 822 of embolic protection filter 814. In use, joint 856 permits rotation of the embolic protection filter within the patient's body while substantially preventing movement of the intravascular device along the guidewire 14.

A placement tube 826 may be utilized to advance the shape memory tube 812 and embolic protection filter 814 along the guidewire 14, and to actuate the shape memory tube 812 between the unlocked and locked positions. Placement tube 826 has a proximal end (not shown), a distal end 830, and an inner lumen 828. The inner lumen 828 is configured in size and shape to radially compress the shape memory tube 812 therein, allowing the anchoring mechanism 810 to slide and rotate about the guidewire 14. To engage the anchoring mechanism 810 along the guidewire 14, placement tube 826 can be withdrawn proximally, allowing the shape memory tube

812 to revert to its pre-defined shape and frictionally engage the guidewire 14, as shown in Figure 19.

To disengage the anchoring mechanism 810 from the guidewire 14, placement tube 826 is advanced distally until the distal end 830 is located proximate and proximal the proximal end 820 of shape memory tube 812. Continued advancement of the placement tube 826 distally causes the shape-memory tube 812 to radially compress within inner lumen 828 and disengage from the guidewire 14. The distal end 830 of shape memory tube 812 may be flared slightly to facilitate advancement of the placement tube 826 about the shape memory tube 812.

Figure 20 illustrates an anchoring mechanism 910 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 910 comprises a proximal end portion 922 of an embolic protection filter (not shown) containing an expandable lumen 958 having an inlet port 960 and an expandable balloon 962. A pressure source 926 in fluid communication with the inlet port 960 is adapted to provide fluidic pressure to the expandable balloon 962 to actuate the device between the unlocked and locked positions.

As shown in Figure 21, when fluidic pressure from pressure source 926 is applied to inlet port 960, balloon 962 expands within expandable lumen 958 forcing the innermost portion 964 of the expandable lumen 958 to deflect inwardly and engage the guidewire 14. To disengage the anchoring mechanism 910 from the guidewire 14, fluid is evacuated from the balloon 962, causing the innermost portion 962 of the expandable lumen 958 to disengage from the guidewire 14.

Figure 22 illustrates an anchoring mechanism 1010 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 1010 comprises a proximal portion 1022 of an embolic protection filter (not shown) having a deflectable section 1012 thereon actuatable between an unlocked (*i.e.* disengaged) position and a locked (*i.e.* engaged) position.

Deflectable section 1012 has a relatively small outer diameter, allowing the deflectable section 1012 to deflect radially and compress along the guidewire 14 when an elastomeric O-ring 1062 is disposed thereon. One or more notches 1066 disposed at various locations along the inner diameter of deflectable section 1012 may also be employed to engage the deflectable section 1012 along the guidewire 14.

In a first position shown in Figure 22, deflectable section 1012 is disengaged from the guidewire 14, allowing the intravascular device to slide and rotate about the

guidewire 14. To engage the anchoring mechanism 1010 along the guidewire 14, a push tube 1068 is positioned proximate and proximal the proximal end 1020 of the intravascular device. Holding the intravascular device stationary with push tube 1068, a placement tube 1026 having an inwardly facing tab 1030 is withdrawn proximally, forcing the O-ring 1062 to slide proximally to a second position about the deflectable section 1012, as shown in Figure 23. The inward force exerted by the O-ring 1062 forces the deflectable section 1012 to bend inwardly and compress against the guidewire 14.

Figure 24 illustrates an anchoring mechanism 1110 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 1110 comprises a placement tube 1126, a push tube 1168 and a plurality of radial tabs 1112 extending from the proximal portion 1122 of an embolic protection filter (not shown). The deflectable radial tabs 1112 are biased inwardly such that when unconstrained by push tube 1168, the radial tabs 1112 deflect inwardly towards the guidewire 14.

Push tube 1168 includes a tapered distal end 1170 having a size and shape that corresponds with the size and shape of the deflectable radial tabs 1112. The placement tube 1126 includes one or more inwardly facing tabs 1130 that can be utilized to transport the anchoring mechanism 1110 along the guidewire 14, and to subsequently release the anchoring mechanism 1110 once engaged.

To engage the anchoring mechanism 1110 along the guidewire 14, push tube 1168 is retracted proximally until the deflectable radial tabs 1112 are unconstrained by the tapered distal end 1170 of push tube 1168. Once unconstrained, the radial tabs 1112 deflect inwardly and frictionally engage the guidewire 14, as shown in Figure 25. Once engaged, the placement tube 1126 can then be retracted proximally, causing the embolic protection filter to deploy within the patient's vessel.

To disengage the anchoring mechanism 1110 from the guidewire 14, placement tube 1126 is advanced distally until the one or more tabs 1130 are positioned proximate and proximal a corresponding tab 1172 located on the embolic protection filter. Continued advancement of the placement tube 1126 distally causes the one or more inwardly facing tabs 1130 to bend slightly, allowing the one or more radial tabs 1130 to displace distal the corresponding tab 1172 located on the embolic protection filter. The push tube 1168 can then be advanced distally, forcing the deflectable radial tabs 1112 to disengage the anchoring mechanism 1110 from the guidewire 14.

Figure 26 illustrates an anchoring mechanism 1210 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 1210 comprises a circular object 1212, a placement tube 1226 having an opening 1230 adapted to contain the circular object 1212, and two recesses 1274, 1276 disposed on the proximal portion 1222 of an embolic protection filter (not shown). The anchoring mechanism 1210 is slidably and rotationally disposed along the guidewire 14 when the circular object 1212 is engaged within the first (*i.e.* larger) recess 1274, and releasably secured to the guidewire 14 when the circular object 1212 is engaged within the second (*i.e.* smaller) recess 1276.

In a first position illustrated in Figure 26, the circular object 1212 is disposed within the first recess 1274. The first recess 1274 is configured in size and shape to allow the circular object 1212 to rotate therein, allowing the anchoring mechanism 1210 to be moved along the guidewire 14. To engage the anchoring mechanism 1210 along the guidewire 14, placement tube 1226 is withdrawn proximally until the circular object 1212 engages the second recess 1276, as shown in Figure 27. The second recess 1276 has a smaller inner diameter such that, when the circular object 1212 is retracted from the first recess 1274 to the second recess 1276, the circular object 1212 compresses against the guidewire 14.

Figure 28 illustrates an anchoring mechanism 1310 in accordance with yet another exemplary embodiment of the present invention employing a flared collet 1312. As shown in Figure 28, the flared collet 1312 includes a reduced inner diameter distal portion 1336 that permits the collet 1312 to deflect inwardly and frictionally engage the guidewire 14 when compressed radially by a placement tube 1326.

To engage the collet 1312 along the guidewire 14, placement tube 1326 is advanced distally, forcing the distal portion 1336 of the collet 1312 to bend inwardly and frictionally engage the guidewire 14, as shown in Figure 29. To disengage the collet 1312 from the guidewire 14, the placement tube 1326 is retracted proximally until the distal portion 1336 disengages from the guidewire 14.

In an alternative embodiment illustrated in Figure 30, the inner diameter of placement tube 1326 may include threads adapted to engage a corresponding set of threads disposed on the outer diameter of the collet 1312. To engage the collet 1312 along the guidewire 14, placement tube 1326 is rotated until the threads on the placement tube 1326 engage the threads on the collet 1312. Continued rotation of the

placement tube 1326 relative to the collet 1312 causes the collet 1312 to frictionally engage the guidewire 14 in a manner similar to that described with respect to Figure 29.

Figure 31 illustrates an anchoring mechanism 1410 in accordance with another exemplary embodiment of the present invention utilizing an offset block. Clamping mechanism 1410 comprises a tubular member 1412 having a plurality of radially offset tabs 1478 extending inwardly towards the guidewire 14. The offset tabs 1478 are staggered at various locations along the inner diameter of the tubular member 1412. In use, the radially offset tabs 1478 prevent movement of the anchoring mechanism 1410 along the guidewire 14 in the absence of a force applied thereto by the operator.

Figure 32 illustrates yet another exemplary embodiment of the present invention utilizing a split jawed collet operatively coupled to a spring seat. As shown in a locked position in Figure 32, anchoring mechanism 1510 comprises a proximal portion 1522 of an embolic protection filter having an inner lumen 1528 configured to receive the guidewire 14.

Secured within the inner lumen 1528 of proximal portion 1522 is a spring 1512 that is frictionally engageable along guidewire 14 in a locked position, and slidably and rotationally disposed about guidewire 14 in an unlocked position. Spring 1512 may be formed from a laser cut tube comprised of a shape memory material such as Nitinol. Alternatively, spring 1512 may be formed from a metal such as 303 or 316 stainless steel. In some embodiments, spring 1512 may be formed from a highly radiopaque material (e.g. 316L stainless steel or platinum) to permit fluoroscopic monitoring of the device.

A split jawed collet 1536 disposed about a spring seat 1582 formed on the proximal portion 1522 of the embolic protection filter may be used to actuate the spring 1512 between the locked and unlocked positions. Split jawed collet 1536 can be formed from a split tubular member, similar to that shown with respect to Figures 28-29. In a locked position illustrated in Figure 32, the split jawed collet 1536 compresses between several notches 1584 formed on seat 1582, which biases the spring 1512 axially, forcing the spring 1512 to frictionally engage the guidewire 14.

To disengage the spring 1512 from the guidewire 14, the operator advances a retrieval sheath 1526 having one or more retrieval fingers 1530 distally until the one or more retrieval fingers 1530 lock onto a first enlarged outer diameter section 1582

formed on proximal portion 1522, as shown in Figure 33. The one or more retrieval fingers 1530 are configured to bend in only a single direction, allowing the retrieval sheath 1526 to lock onto the proximal portion 1522 of the embolic protection filter. The one or more retrieval fingers 1530 may be formed from any number of suitable materials such as Nitinol, nylon, polyether-ether ketone (PEEK), etc.

Once the retrieval sheath 1526 is engaged along the proximal portion 1522 of the filter, the operator next advances a second sheath 1584 along the guidewire until a second set of retrieval fingers 1586 engage a second enlarged outer diameter section 1588 formed on proximal portion 1522. Once the second set of retrieval fingers 1586 engage the second enlarged outer diameter section 1588, a push tube 1568 is advanced distally, forcing the split jaw collet 1536 to compress axially, causing the spring 1512 to frictionally disengage from the guidewire, as shown in Figure 34. The embolic protection filter can then be retracted along guidewire 14 and removed from the patient's body, if desired.

Figure 35 illustrates an anchoring mechanism 1610 in accordance with yet another exemplary embodiment of the present invention utilizing a sleeve 1612. Anchoring mechanism 1610 comprises a proximal portion 1622 of an embolic protection filter (not shown) having an inner lumen 1628 configured to receive the guidewire 14.

A spring 1662 attached to the proximal portion 1622 can be utilized to frictionally engage the sleeve 1612 along the guidewire 14. Spring 1662 has a proximal end 1634 and a distal end 1636. The proximal end 1634 of spring 1662 is attached to a tubular member 1690 slidably disposed along guidewire 14. The distal end 1636 of spring 1662 is fixedly attached to the proximal portion 1622 of the embolic protection filter.

Sleeve 1612 may be formed from a loosely braided material such as Dacron, and is configured to radially collapse when placed under tension by the spring 1662. The sleeve 1612 is secured at a distal end 1618 to the proximal portion 1622 of the filter. The proximal end 1620 of the sleeve, in turn, is attached to the tubular member 1690. In a locked position illustrated in Figure 35, the spring 1662 forces the sleeve 1612 into tension axially, forcing the sleeve 1612 to radially compress and frictionally engage the guidewire 14.

To disengage the sleeve 1612 from the guidewire 14, the operator advances a retrieval sheath 1626 having one or more retrieval fingers 1630 distally along the

guidewire 14 until the one or more retrieval fingers 1630 lock onto a first notch 1682 located on the proximal portion 1622, as shown in Figure 36. Once the retrieval sheath 1626 is engaged along the proximal portion 1622 of the filter, the operator next advances a second sheath 1684 along the guidewire 14 until a second set of retrieval fingers 1686 engage a second notch 1688 formed on the outer diameter of proximal portion 1622 proximal the first notch 1682. Once the second set of retrieval fingers 1686 engage the second notch 1688, a push tube 1668 is advanced along the guidewire 14, forcing the spring 1662 into compression, and causing the sleeve 1612 to radially expand and disengage from the guidewire 14, as shown in Figure 37.

Figure 38 illustrates an anchoring mechanism 1710 in accordance with yet another exemplary embodiment of the present invention. Anchoring mechanism 1710 comprises a tubular member 1712 slidably and rotationally disposed about a guidewire 14, a locking tube 1726, and a filter mount 1722. Tubular member 1712 has a proximal end 1734, a distal end 1736, and an inner lumen 1728 configured to receive the guidewire 14. The filter mount 1722, which forms the proximal portion of an embolic protection filter (not shown), is slidably and rotationally disposed about the tubular member 1712. The distal end 1736 of tubular member 1712 is flared slightly such that, in use, the filter mount 1722 is prevented from sliding off the distal end 1736 of the tubular member 1712. If desired, the filter mount 1722 may be formed of a radiopaque material such as stainless steel, gold or platinum to enable the operator to fluoroscopically judge the location of the device within the patient's body.

Tubular member 1712 further includes one or more latches 1792 adapted to frictionally engage the guidewire 14 when actuated. The latches 1792 may be formed by cutting the tubular member 1712 at various locations along its length and/or radius. The proximal end 1720 of each latch 1792 is attached to the tubular member 1712, and acts as a pivot to permit the latches 1792 to bend inwardly towards the guidewire 14. The distal end 1718 of each latch 1792, in turn, is bent at an angle of approximately 90°, forming a contact surface to frictionally engage the guidewire 14. A slight upward deflection is heat set into each latch 1792 to permit the tubular member 1712 to slide along the guidewire 14 when unconstrained radially.

A locking tube 1726 may be utilized to frictionally engage the one or more latches 1792 along the guidewire 14. Locking tube 1726 has an inner diameter slightly larger than the outer diameter of tubular member 1712, allowing the tube 1726 to slide over the tubular member 1712 to engage the one or more latches 1792.

To frictionally engage the guidewire 14, the locking tube 1726 is advanced distally along the guidewire 14 to a location proximate and proximal the proximal end 1734 of tubular member 1712. Continued advancement of the locking tube 1726 distally forces the latches 1792 to rotate inwardly and frictionally engage the guidewire 14, as shown in Figure 39.

To subsequently disengage the latches 1792 from the guidewire 14, a retrieval system similar to that described with respect to Figures 35-37 may be employed. For example, as shown in Figure 39, a retrieval sheath 1726 having one or more retrieval fingers 1730 may be advanced along the guidewire 14 and secured to the filter mount 1722 at a first notch 1782. Once engaged, a second sheath 1784 having a second set of retrieval fingers 1786 may be advanced along the guidewire 14 and locked onto a second notch 1788 formed on the locking tube 1726, as shown in Figure 40. The second sheath 1784 can be retracted proximally until the one or more latches 1792 are unconstrained radially, allowing the tubular member 1712 to slide and rotate along the guidewire 14. The operator can then retract the second sheath 1784 proximally, causing the one or more latches 1792 to disengage from the guidewire 14.

Figure 41 illustrates an anchoring mechanism 1810 in accordance with yet another exemplary embodiment of the present invention utilizing a wedge. Anchoring mechanism 1810 comprises an object 1812 that is slidably and rotationally disposed about a guidewire 14 in an unlocked position, and releasably secured to the guidewire 14 in a locked position. Object 1812 has a proximal section 1820 and a distal section 1818. The proximal section 1820 of object 1712 is configured to bend or flex inwardly towards the guidewire 14 when compressed radially by a wedge 1894.

In the exemplary embodiment illustrated in Figure 41, object 1812 tapers distally, having a smaller outer diameter on proximal section 1820 than on the distal section 1818. One or more notches 1882 disposed within the outer surface of the object 1812 further permit the proximal section 1820 to bend or flex inwardly when wedge 1894 is advanced thereon.

The distal section 1818 of object 1812 may further optionally include a joint 1856 adapted to permit rotation of the object 1812 relative to the proximal portion 1822 of the embolic protection filter 1814. In use, joint 1856 permits rotation of the embolic protection filter 1814 within the vessel while substantially preventing movement of the anchoring mechanism 1810 along the guidewire 14.

To frictionally engage the object 1812 along the guidewire 14, a push tube 1868 can be advanced distally, forcing the wedge 1894 to slide along the object 1812. A sheath 1826 having a force-calibrated tab 1830 adapted to bend in only one direction in response to a sufficient force exerted thereon can be utilized to hold the object 1812 in place when advancing the wedge 1894. Continued movement of the wedge 1894 relative to the object 1812 causes the object 1812 to compress radially, forcing the proximal section 1820 to bend inwardly and frictionally engage the guidewire 14. Once engaged, the retrieval sheath 1826 can be withdrawn proximally until the force-calibrated tab 1830 bends and compresses against the wedge 1894, and until the embolic protection filter 1814 is deployed within the vessel, as shown in Figure 42. The push tube 1868 can then be withdrawn proximally from the body, if desired.

In an alternative embodiment illustrated in Figures 43-45, an anchoring mechanism 1910 in accordance with the present invention may include an object 1912 that tapers proximally. As shown in Figure 43, object 1912 has a larger outer diameter on the proximal section 1920 than on the distal section 1918. The proximal section 1920 is configured to bend or flex inwardly towards the guidewire 14 when compressed radially by a wedge 1994. One or more notches 1982 disposed within the outer surface of the object 1912 further permit the proximal section 1920 to bend or flex inwardly when wedge 1994 is advanced thereon.

In a first (unlocked) position illustrated in Figure 43, object 1912 is slidably and rotationally disposed about the guidewire 14. To frictionally engage the object 1912 along the guidewire 14, a push tube 1968 is advanced distally against the object 1912, forcing the object 1912 to slide relative to the wedge 1994, as shown in Figure 44. A sheath 1926 having a force-calibrated tab 1930 adapted to bend in only one direction in response to a sufficient force exerted thereon can be utilized to hold the wedge 1994 stationary when advancing the object 1912 via the push tube 1968. Continued advancement of the push tube 1968 distally, or in the alternative, retraction of the retrieval sheath 1926 proximally, causes the force-calibrated tab 1930 to bend and compress against the wedge 1994, as shown in Figure 45.

In an alternative embodiment illustrated in Figures 46-47, an anchoring mechanism 2010 in accordance with the present invention may include a push tube 2068 having threads configured to engage a corresponding set of threads disposed on the wedge 2094. Anchoring mechanism 2010 comprises an object 2012 having a

proximal section 2020 and a distal section 2018, a retrieval sheath 2026, a wedge 2094, and a push tube 2068. The object 2012 tapers proximally, and forms the proximal portion of an embolic protection filter 2014. The proximal section 2020 of object 2012 is configured to bend or flex inwardly towards the guidewire 14 when compressed radially by the wedge 2094.

In the exemplary embodiment illustrated in Figures 46-47, wedge 2094 includes threads on its outer diameter configured to mate with a corresponding set of threads disposed on a reduced inner diameter distal portion 2070 of the push tube 2068.

To frictionally engage the object 2012 along the guidewire 14, push tube 2068 is retracted proximally, forcing the proximal section 2020 of the object 2012 to bend inwardly and frictionally engage the guidewire 14. Once engaged, the retrieval sheath 2026 may be withdrawn proximally, causing the force-calibrated tab 2030 to bend and compress against the wedge 2094, as shown in Figure 47.

Figure 48 illustrates an anchoring mechanism 2110 in accordance with yet another exemplary embodiment of the present invention utilizing a slotted tube. As shown in Figure 48, anchoring mechanism 2110 comprises a slotted tube 2112 having an inner lumen 2114 configured to slidably receive a guidewire (not shown). As with any of the previous embodiments, the slotted tube 2112 may form the proximal portion of an embolic protection filter, or may act as a proximal stop to prevent proximal movement of the filter along the guidewire.

In the exemplary embodiment illustrated in Figure 48, slotted tube 2112 comprises a thin-wall tube formed from a shape-memory material such as Nitinol. Slotted tube 2112 includes a necked-down portion 2116 having an inner diameter that is slightly smaller than the outer diameter of the guidewire. Several slots 2118 located within the necked-down portion 2116 are configured to expand slightly to allow the guidewire to slide within lumen 2114 when the slotted tube 2112 is unconstrained radially. As can be seen in greater detail in Figure 49, the slots 2118 are circumferentially disposed 120° apart from each other, and extend through the wall of the slotted tube 2112.

To expand the slots 2116 in an outward direction, the slotted tube 2112 can be heat treated at an appropriate temperature using, for example, a heater or a laser. Once heated, the slots 2118 deform slightly, allowing the guidewire 14 to be inserted through the slotted tube 2112, as shown in Figure 50. To facilitate heat setting of the

slots 2116, a shape memory material such as Nitinol can be used. In an alternative implementation, the slots 2118 can be formed using an annealed steel or polymeric material. For example, the slots 2116 can be molded to a particular dimension using a polymeric material such as polytetrafluoroethylene, polyvinylchloride or ABS plastic.

To engage the anchoring mechanism 2110 along the guidewire 14, a locking tube 2120 is advanced along the guidewire 14 to a point proximate and proximal the necked-down portion 2116 of slotted tube 2112. The locking tube 2120 has an inner diameter that is slightly larger than the outer diameter of the slotted tube 2112, allowing the locking tube 2120 to be advanced over the slotted tube 2112. To releasably secure the slotted tube 2112 to the guidewire 14, the operator continues to advance the locking tube 2120 distally until the necked-down portion 2116 compresses against the guidewire 14, as shown in Figure 51.

In an alternative embodiment illustrated in Figures 52-56, the slotted tube may include several necked down regions located along its length configured to releasably secure to the guidewire 14. As shown in Figure 52, anchoring mechanism 2210 comprises a slotted tube having a first necked-down region 2216, and a second necked-down region 2220 located distal the first necked-down region 2216. The first necked-down region 2216 includes two slots 2224 circumferentially disposed 180° apart from each other, and that extend through the wall of the slotted tube 2212, as shown in Figure 53. The second necked-down region 2222, in turn, includes two slots 2226 that are radially offset 90° from the slots 2224 on the first necked-down region 2216, as shown in Figure 54.

To engage the anchoring mechanism 2210 along the guidewire 14, a locking tube 2220 similar to that discussed with respect to Figure 51 is advanced along the guidewire 14 to a point proximate and proximal to the first necked-down portion 2216 of slotted tube 2212, as shown in Figure 56. Continued advancement of the locking tube 2220 about the first necked-down portion 2216 compresses the slotted tube 2212 against the guidewire 14, as shown in Figure 51. Further advancement of the locking tube 2220 distally causes the second necked-down portion 2222 to compress against the guidewire 14 in a similar manner.

Although the exemplary embodiment illustrated in Figures 52-56 illustrates two locking portions 2216, 2222 along the length of the slotted tube 2212, it is to be understood that other configurations are possible without deviating from the scope of the invention. For example, a slotted tube having three or more necked-down regions

can be employed. Moreover, the number of slots (e.g. 4, 5, 6, etc.) disposed within each necked-down region can be increased, if desired, to provide a greater number of locations for the slotted tube to frictionally engage the guidewire.

To further increase the frictional force exerted on the guidewire, the inner diameter of the slotted tube may include a roughened surface. The roughened surface may be formed by welding several small beads to the inner surface, sand blasting the inner surface, or by machining small grooves into the inner surface of the slotted tube. The slotted tube may also be formed from a material having a relatively porous surface, thereby increasing the roughness of the surface.

In another alternative embodiment illustrated in Figures 57-59, an anchoring mechanism 2310 in accordance with the present invention may include a slotted tube 2312 comprising one or more portions 2328 having a relatively large section modulus, and one or more portions 2330 having a relatively small section modulus. As shown in a pre-heat treated position in Figure 57, the slotted tube 2312 may include several circumferentially disposed slots 2332 extending through the wall of the slotted tube 2312. The one or more portions 2328 having a relatively large section modulus are configured to distribute the axial force applied to the slotted tube when the embolic protection filter is moved along the guidewire 14. In use, the slots 2332 formed about the slotted tube 2312 are configured to expand slightly to allow the guidewire 14 to slide and rotate within the slotted tube 2312 when unconstrained radially.

As can be seen in Figure 58, the slots 2332 may be formed in a direction substantially parallel to centerline of the slotted tube. The slots 2332 may be heat treated as discussed with respect to the previous embodiment, or may be formed during manufacture. Although the slots 2332 illustrated in Figure 58 are disposed along a line substantially parallel to the centerline of the slotted tube 2312, other configurations are possible. In one embodiment, for example, the one or more slots may be helically disposed about the slotted tube 2312.

To engage the anchoring mechanism 2310 along the guidewire 14, a locking tube 2320 can be advanced along the guidewire 14 to a point proximate and proximal to the necked-down portion 2316 of slotted tube 2312. Continued advancement of the locking tube 2312 distally about the necked-down portion 2316 compresses the slotted tube 2312 against the guidewire 14, as shown in Figure 59. Several protrusions 2334 disposed on the outer diameter of the slotted tube 2312 are configured to frictionally engage the locking tube 2320 against the slotted tube 2312.

Having thus described the several embodiments of the present invention, those of skill in the art will readily appreciate that other embodiments may be made and used which fall within the scope of the claims attached hereto. Numerous advantages of the invention covered by this document have been set forth in the foregoing description. Changes may be made in details, particular in matters of shape, size and arrangement of parts without exceeding the scope of the invention. For example, while several of the embodiments illustrated herein illustrate the attachment of an embolic protection filter to the guidewire, it is to be understood that other intravascular devices may employ the anchoring mechanisms discussed herein. It will be understood that this disclosure is, in many respects, only illustrative.

What is claimed is:

1. An anchoring mechanism for releasably securing an intravascular device to an elongated member disposed within a body lumen, said anchoring mechanism comprising:

an object actuatable between an unlocked position and a locked position, wherein the object is slidably and rotationally disposed about the elongated member in the unlocked position, and is releasably secured to the elongated member in the locked position; and

placement means for actuating said object between the unlocked position and locked position.

2. An anchoring mechanism for releasably securing an intravascular device to an elongated member disposed within a body lumen, said anchoring mechanism comprising:

an object actuatable between an unlocked position and a locked position, wherein, the object is slidably and rotationally disposed about the elongated member in the unlocked position, and is releasably secured to the elongated member in the locked position;

placement means for actuating said object between the unlocked position and locked position; and

retrieval means for disengaging the object from the locked position to the unlocked position.

3. An intravascular device comprising:

an embolic protection filter slidably disposed on a guidewire; and

anchoring means for attaching the embolic protection filter to the guidewire, said anchoring means comprising an anchoring mechanism actuatable between an unlocked position and a locked position, wherein the anchoring mechanism is slidably disposed along the guidewire in the unlocked position, and is releasably secured to the guidewire in the locked position.

4. An intravascular device comprising:

an embolic protection filter slidably disposed on a guidewire;

anchoring means for attaching the embolic protection filter to the guidewire, said anchoring means comprising an object actuatable between an unlocked position and a locked position, wherein the anchoring mechanism is slidably disposed along the guidewire in the unlocked position, and is releasably secured to the guidewire in the locked position; and

placement means for actuating said anchoring mechanism between the unlocked position and locked position.

5. An anchoring mechanism for releasably securing an intravascular device to an elongated member disposed within a body lumen, said anchoring mechanism comprising an object actuatable between an unlocked position and a locked position, wherein the object is slidably and rotationally disposed about the elongated member in the unlocked position, and is releasably secured to the elongated member in the locked position.

6. The anchoring mechanism of claim 5, wherein said elongated member is a guidewire.

7. The anchoring mechanism of claim 5, wherein said elongated member is a catheter.

8. The anchoring mechanism of claim 5, wherein said object comprises a spring coil having a proximal portion and a distal portion.

9. The anchoring mechanism of claim 8, wherein the proximal portion of said spring coil extends proximally in a U-shape configuration such that when unconstrained radially, the spring coil is releasably secured to the elongated member.

10. The anchoring mechanism of claim 5, wherein said object comprises a split tube segment.

11. The anchoring mechanism of claim 5, wherein said object comprises one or more leaf clamps.

12. The anchoring mechanism of claim 5, wherein said object comprises one or more wires.

13. The anchoring mechanism of claim 5, wherein said object comprises a helical spring.

14. The anchoring mechanism of claim 5, wherein said object comprises a cam.

15. The anchoring mechanism of claim 5, wherein said object comprises an elastomeric object.

16. The anchoring mechanism of claim 5, wherein said object comprises a shape memory tube.

17. The anchoring mechanism of claim 5, wherein said object comprises an expandable balloon.

18. The anchoring mechanism of claim 5, wherein said object comprises an O-ring.

19. The anchoring mechanism of claim 5, wherein said object comprises a plurality of deflectable radial tabs.

20. The anchoring mechanism of claim 5, wherein said object comprises a circular object disposable within several recesses.

21. The anchoring mechanism of claim 5, wherein said object comprises a collet.

22. The anchoring mechanism of claim 21, wherein said collet is a flared collet.

23. The anchoring mechanism of claim 21, wherein said collet is a threaded collet.

24. The anchoring mechanism of claim 5, wherein said object comprises an offset block.

25. The anchoring mechanism of claim 5, wherein said object comprises a split jawed collet operatively coupled to a spring.

26. The anchoring mechanism of claim 5, wherein said object comprises a sleeve operatively coupled to a spring.

27. The anchoring mechanism of claim 5, wherein said object comprises a tubular member having one or more latches.

28. The anchoring mechanism of claim 5, wherein said object comprises a wedge.

29. The anchoring mechanism of claim 28, wherein said wedge is a threaded wedge.

30. The anchoring mechanism of claim 5, wherein said object comprises a slotted tube having at least one necked-down portion.

31. The anchoring mechanism of claim 5, further comprising placement means for actuating said object between the unlocked position and locked position.

32. The anchoring mechanism of claim 31, wherein said placement means comprises a tubular member.

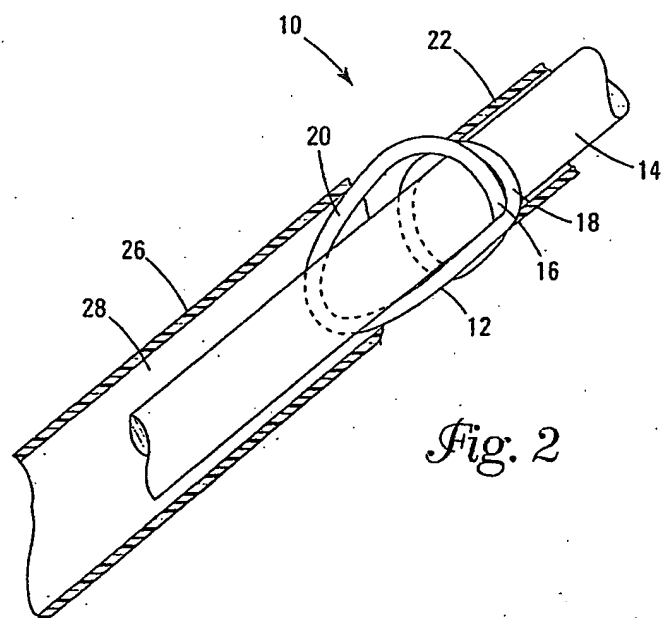
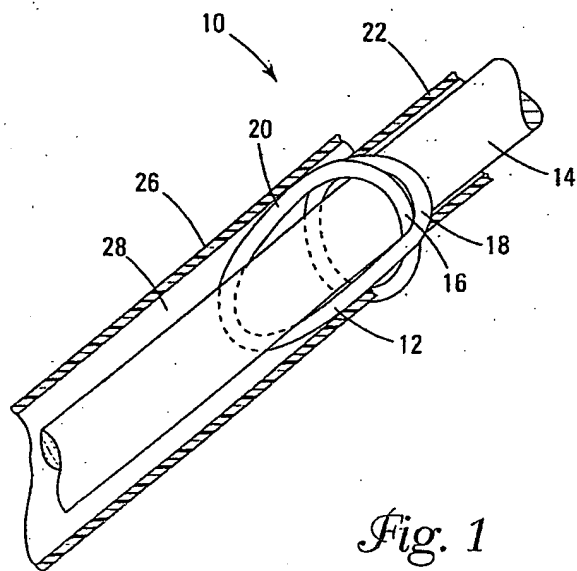
33. The anchoring mechanism of claim 5, further comprising retrieval means for disengaging the object from the locked position to the unlocked position.

34. An anchoring mechanism for releasably securing an intravascular device to an elongated member disposed within a body lumen, said anchoring mechanism comprising:

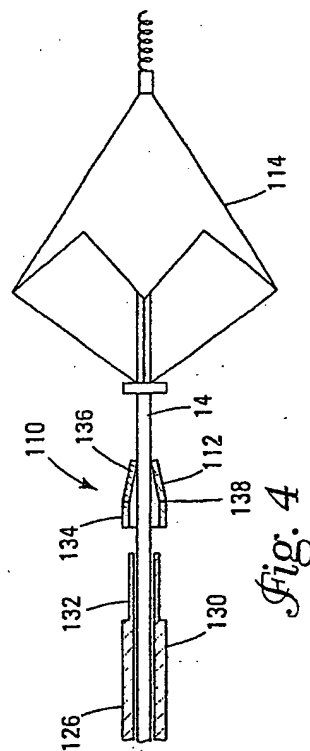
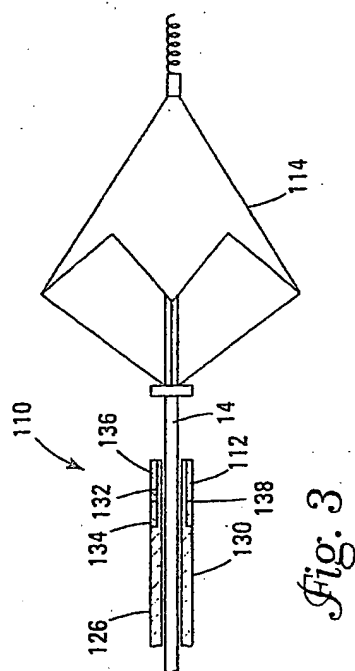
an object actuatable between an unlocked position and a locked position, wherein the object is slidably and rotationally disposed about the elongated member in the unlocked position, and is releasably secured to the elongated member in the locked position; and

placement device actuatable to move said object between the unlocked position and locked position.

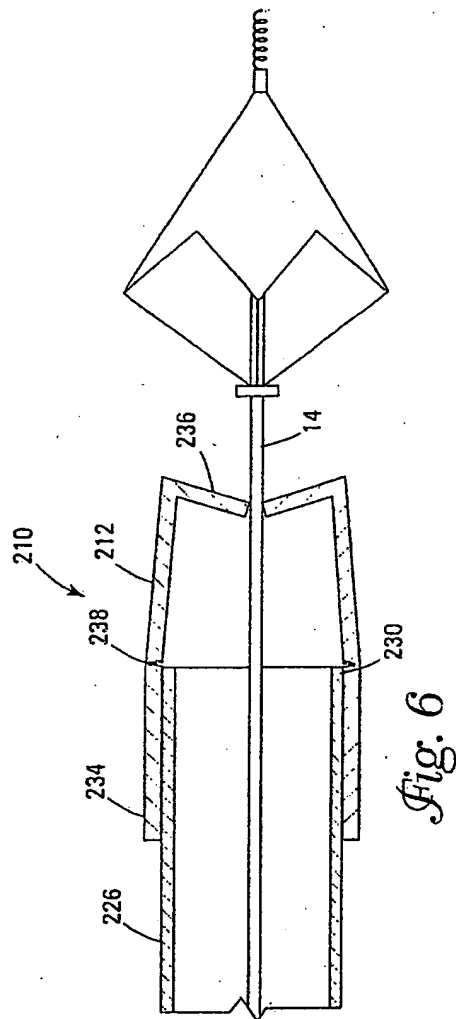
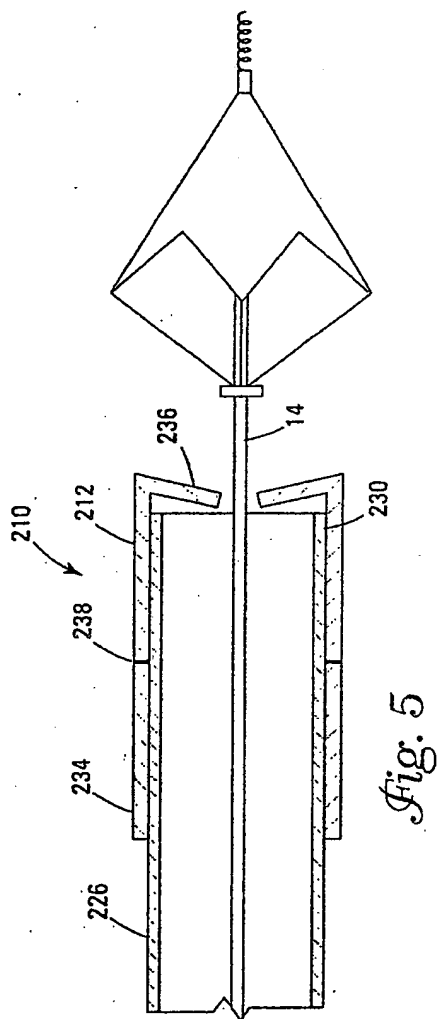
1/24



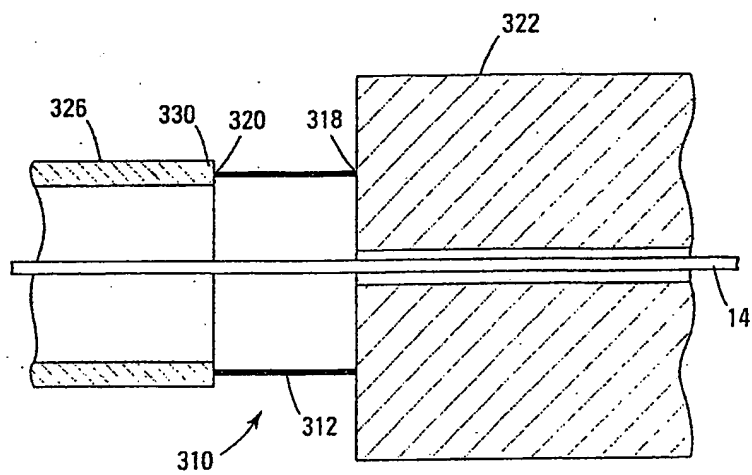
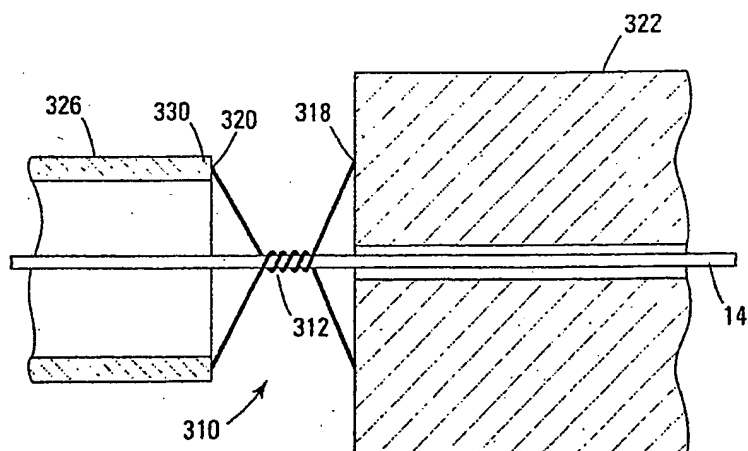
2/24



3/24



4/24

*Fig. 7**Fig. 8*

5/24

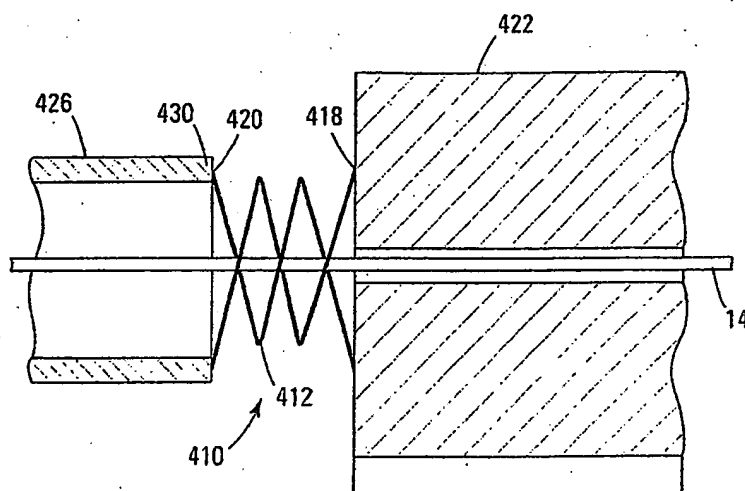


Fig. 9

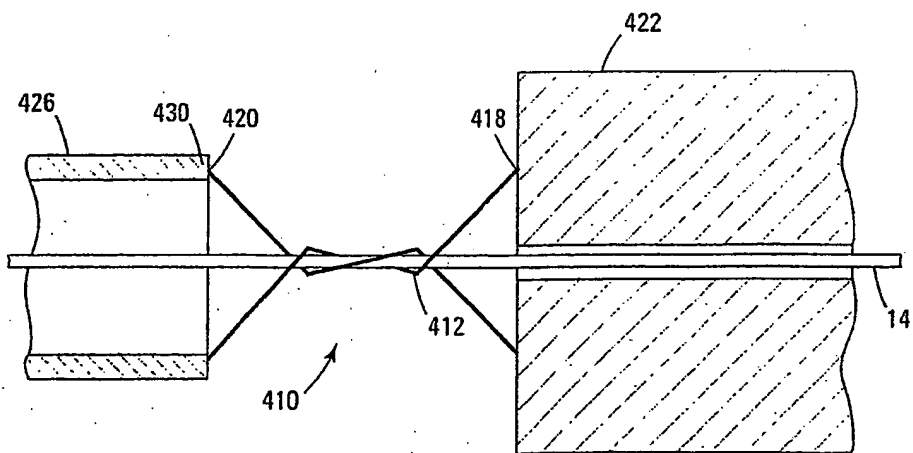


Fig. 10

6/24

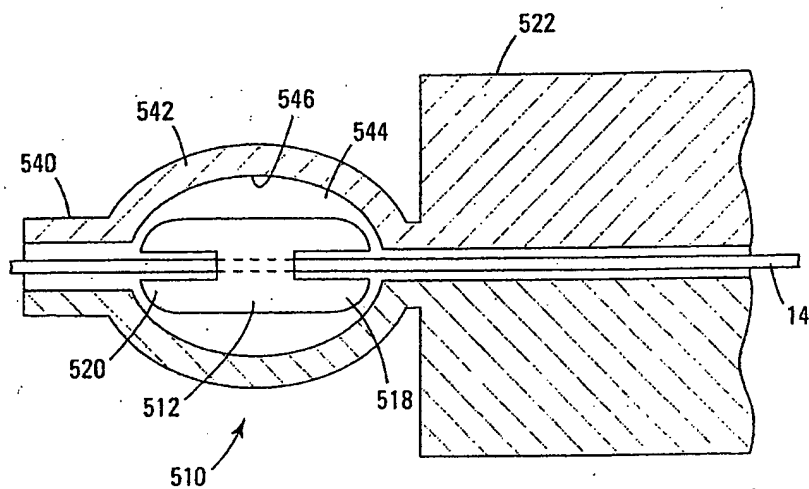


Fig. 11

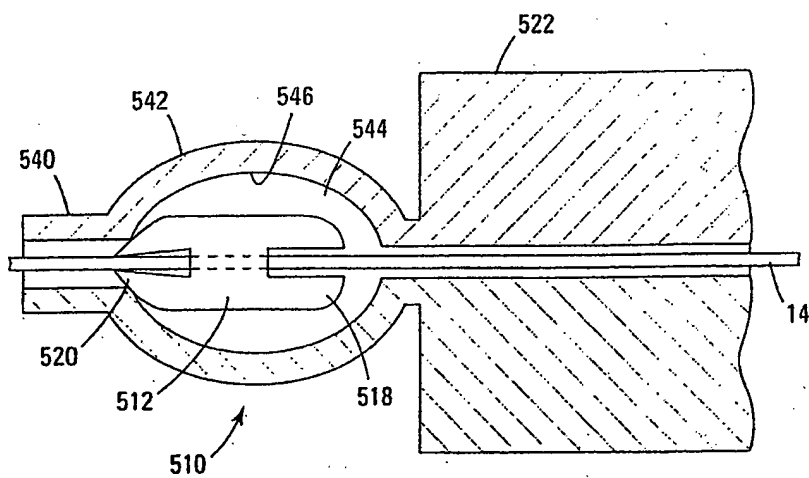


Fig. 12

7/24

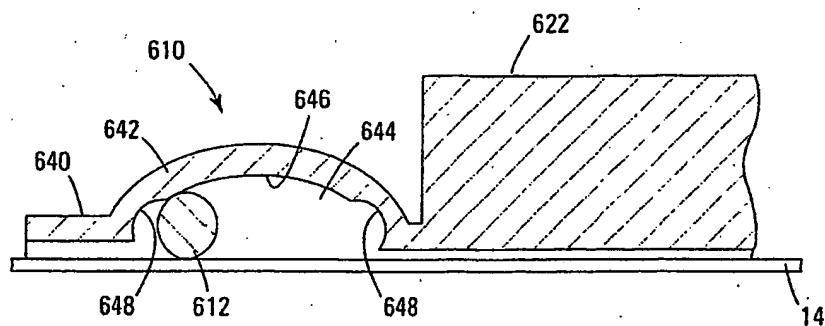


Fig. 13

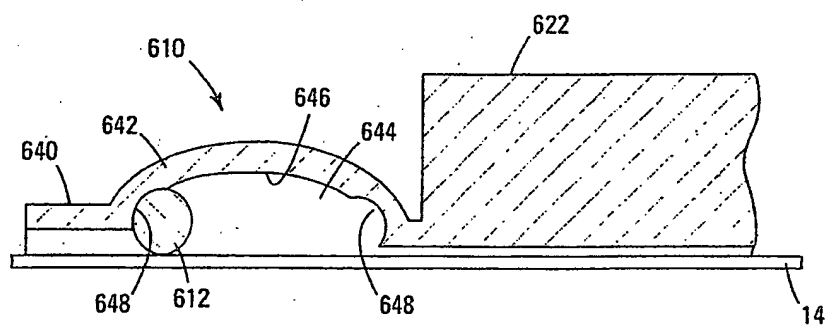


Fig. 14

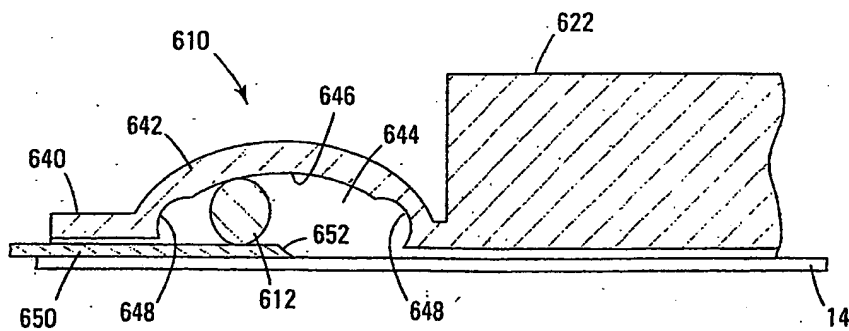
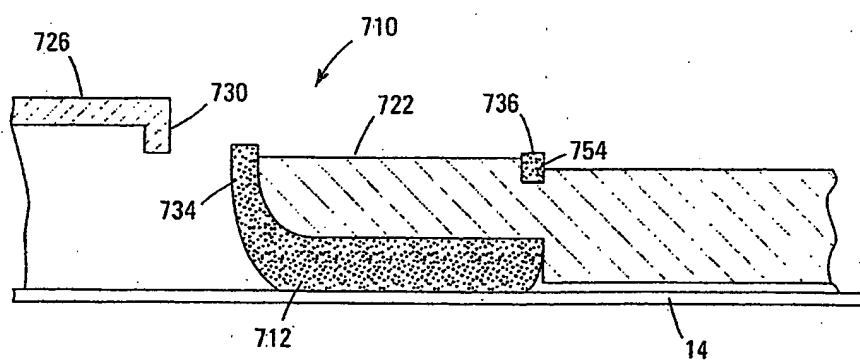
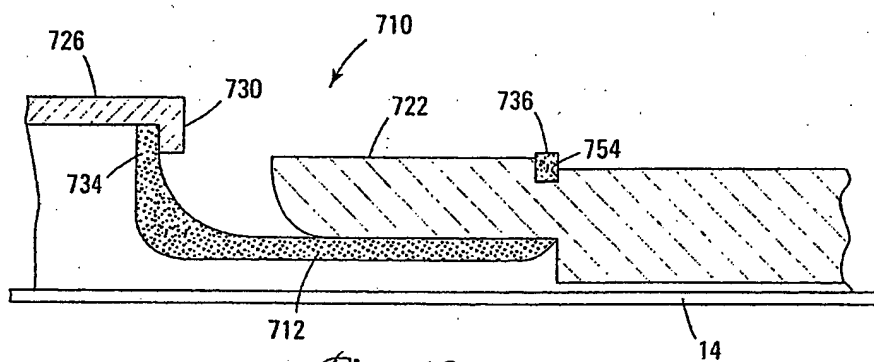


Fig. 15

8/24



9/24

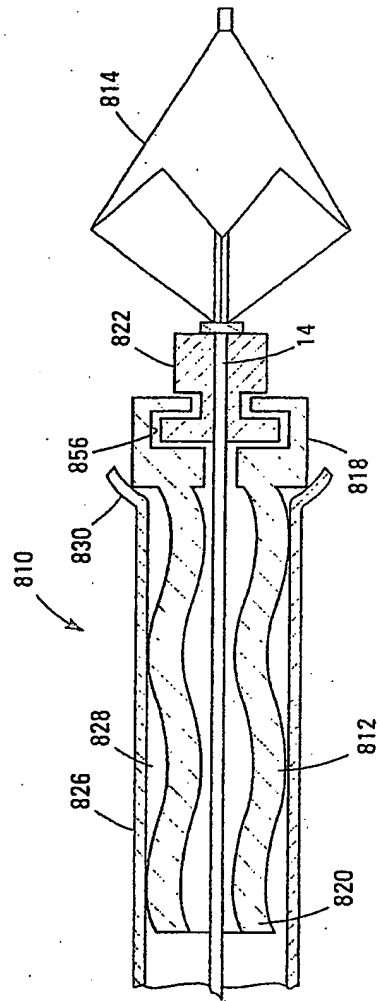


Fig. 18

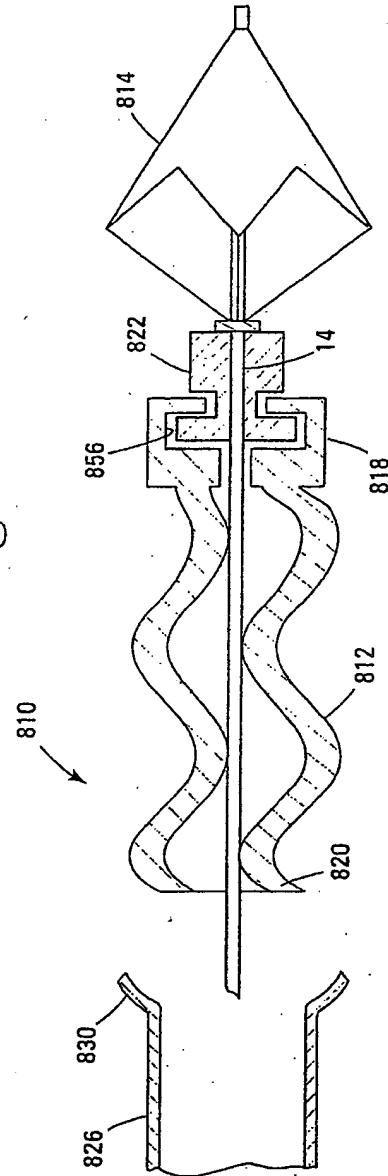


Fig. 19

10/24

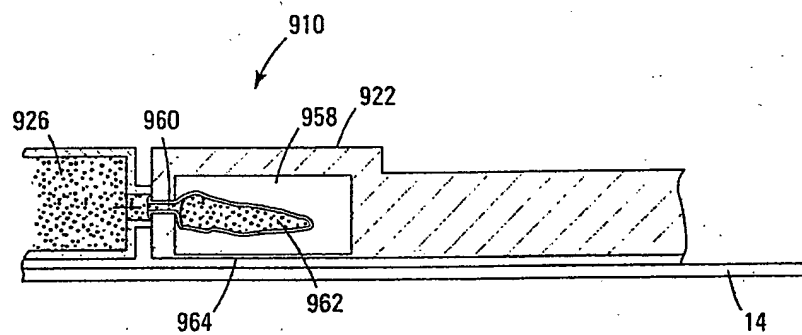


Fig. 20

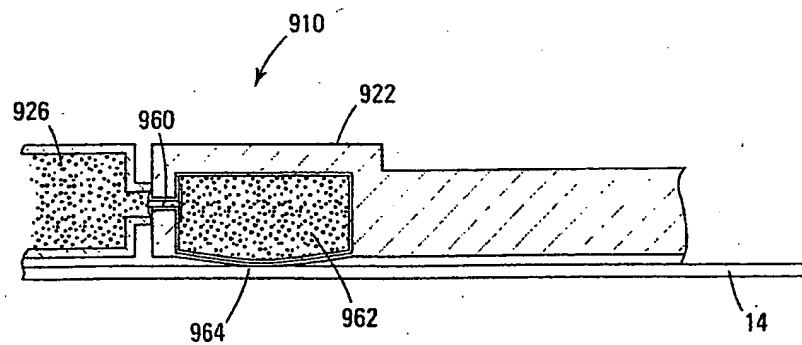
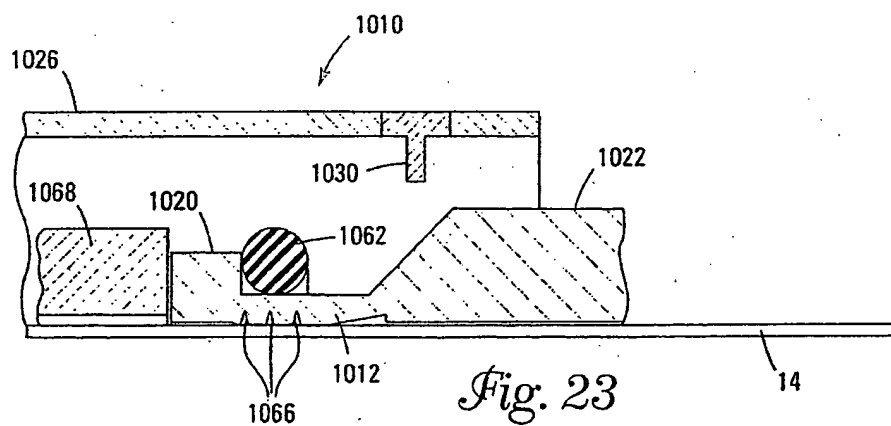
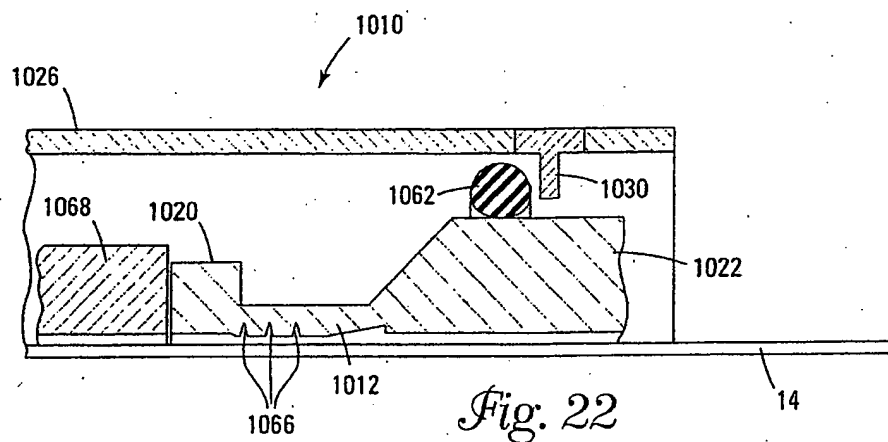
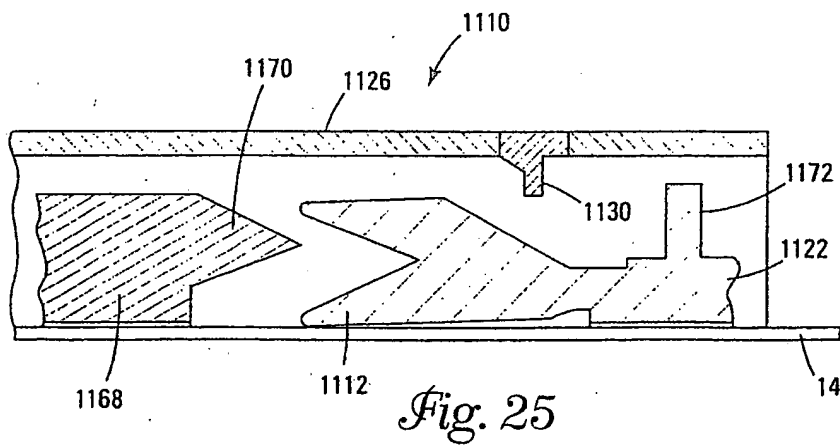
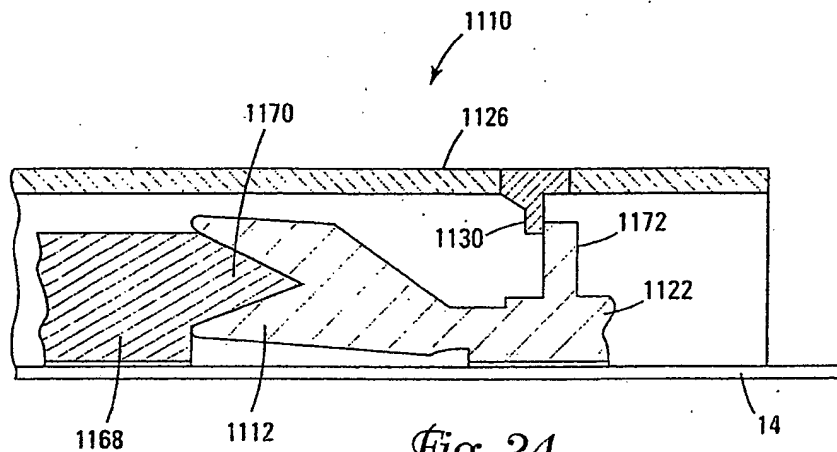


Fig. 21

11/24



12/24



13/24

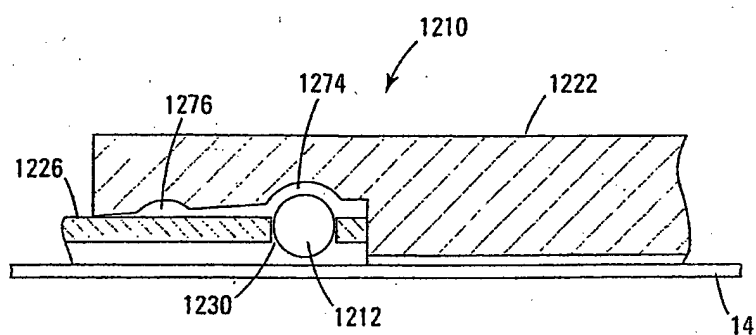


Fig. 26

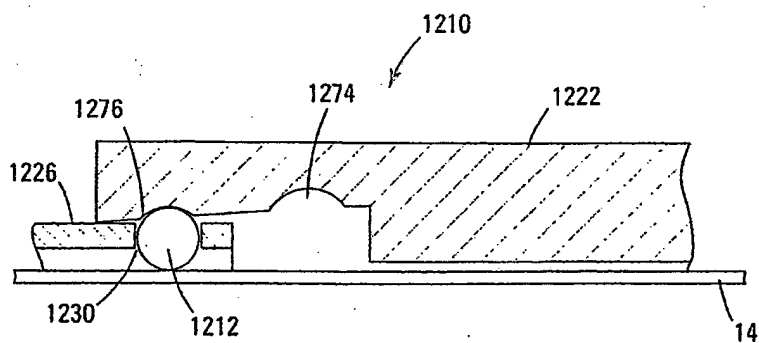
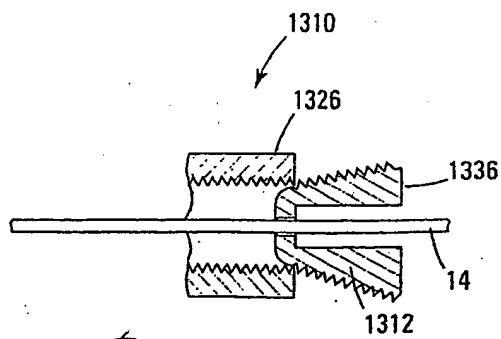
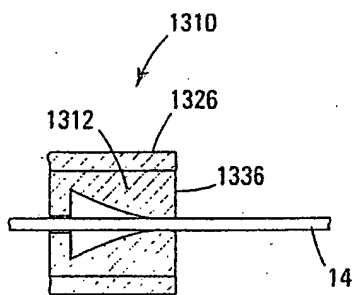
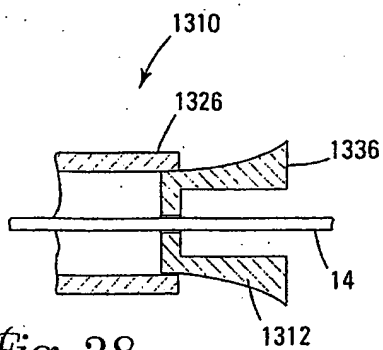


Fig. 27

14/24



15/24

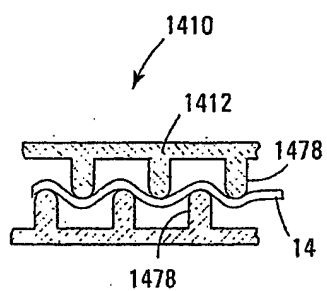


Fig. 31

16/24

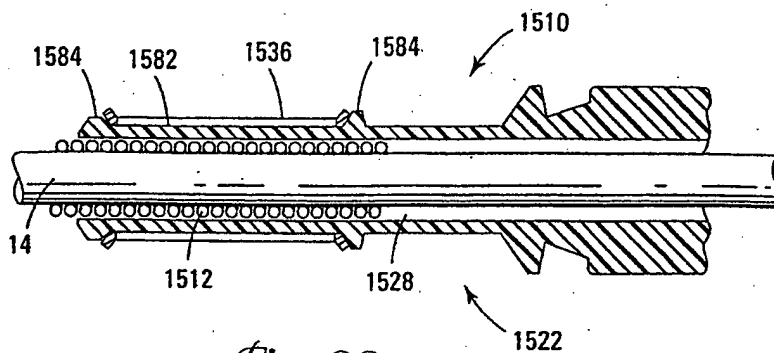


Fig. 32

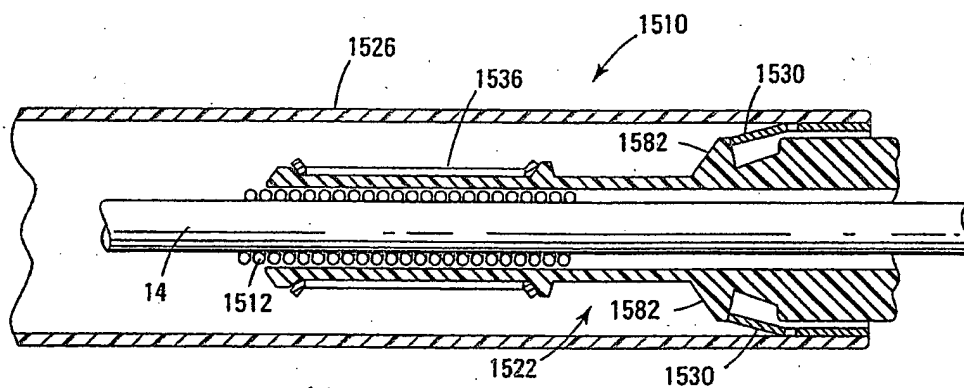


Fig. 33

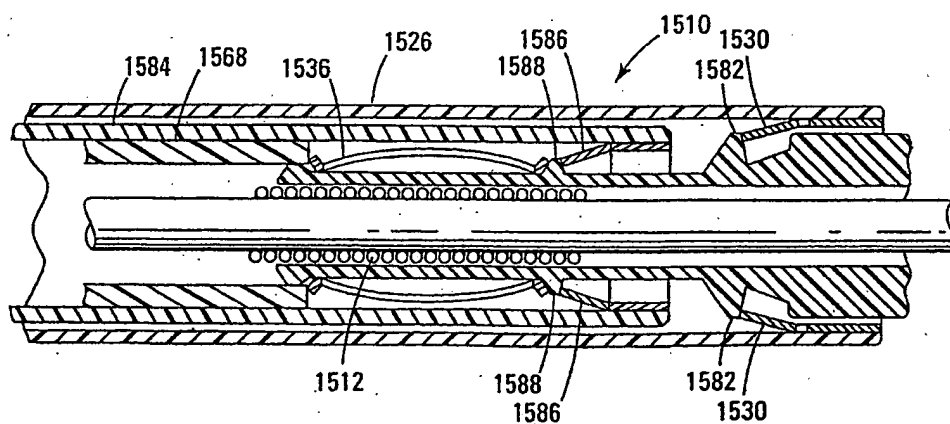


Fig. 34

17/24

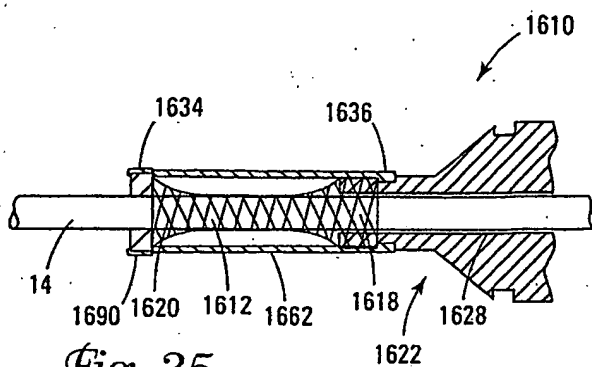


Fig. 35

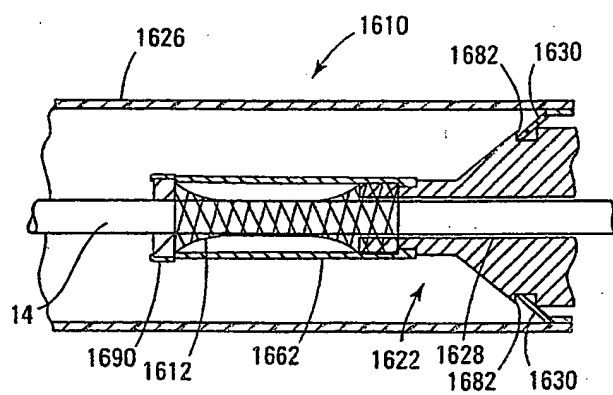


Fig. 36

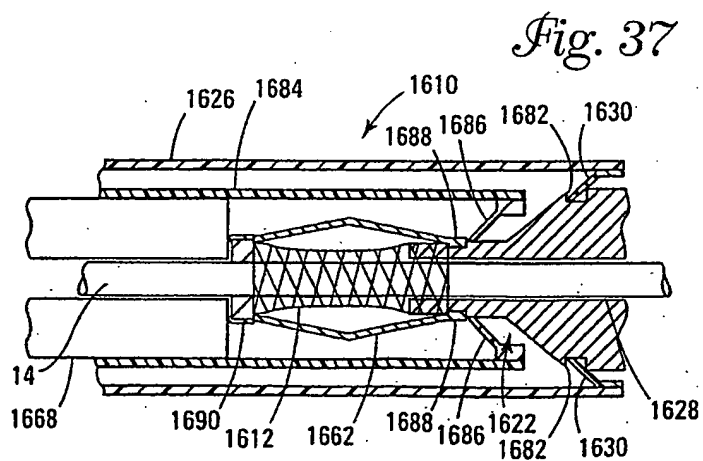


Fig. 37

18/24

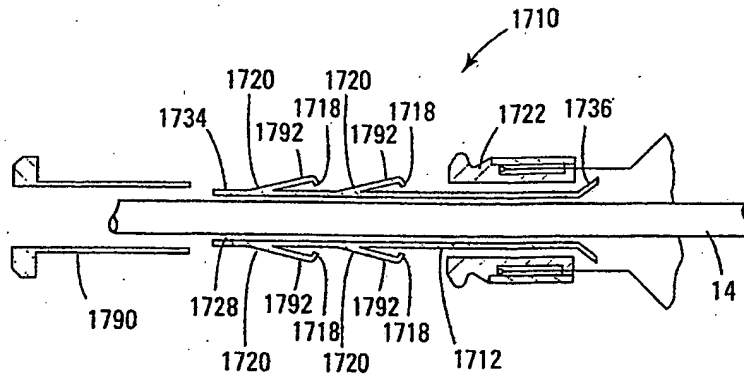


Fig. 38

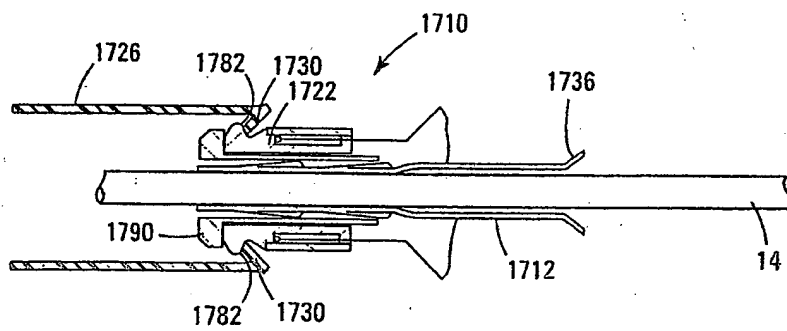


Fig. 39

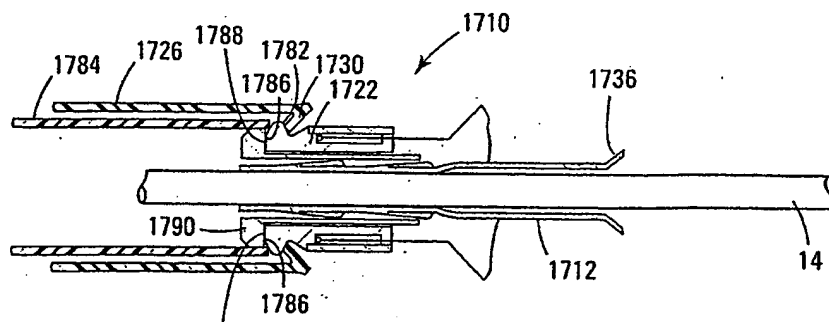
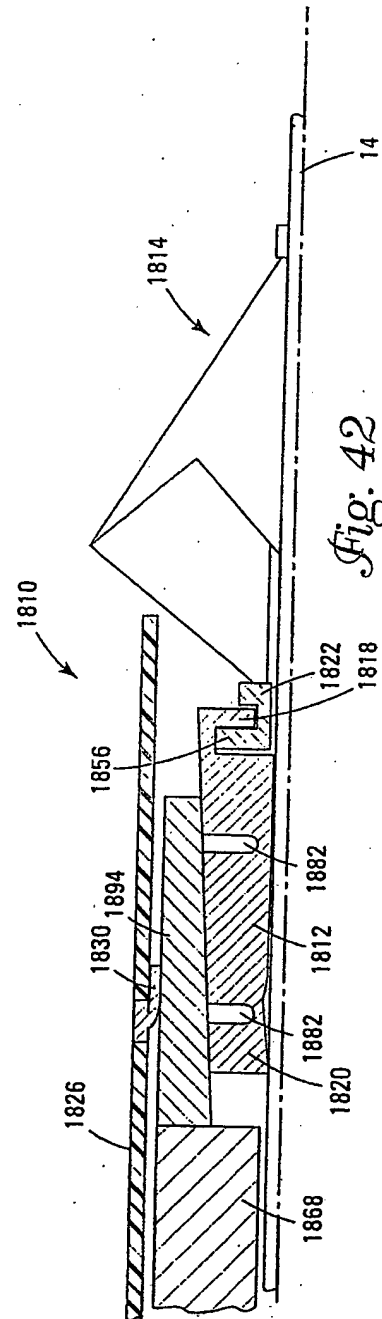
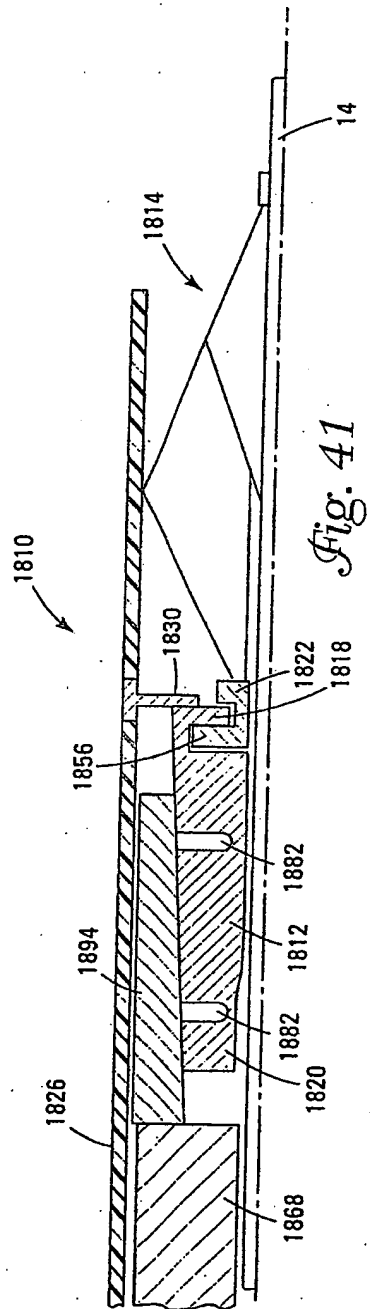
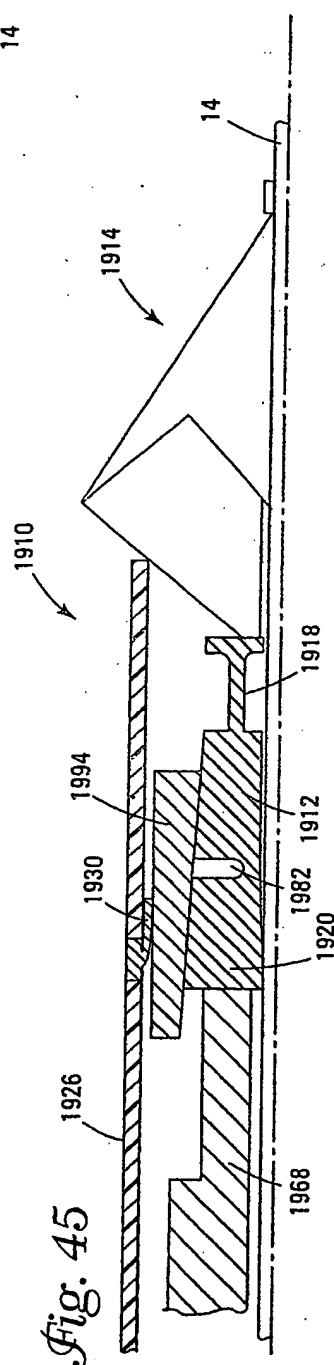
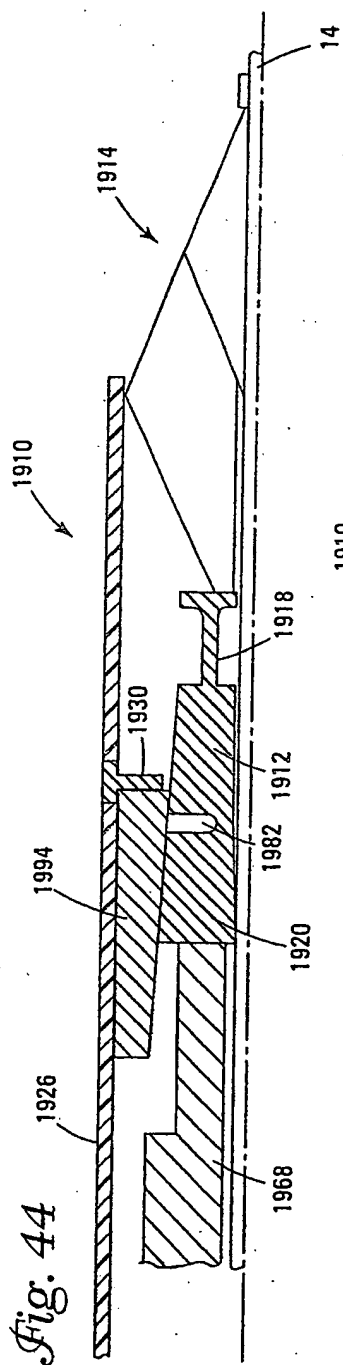
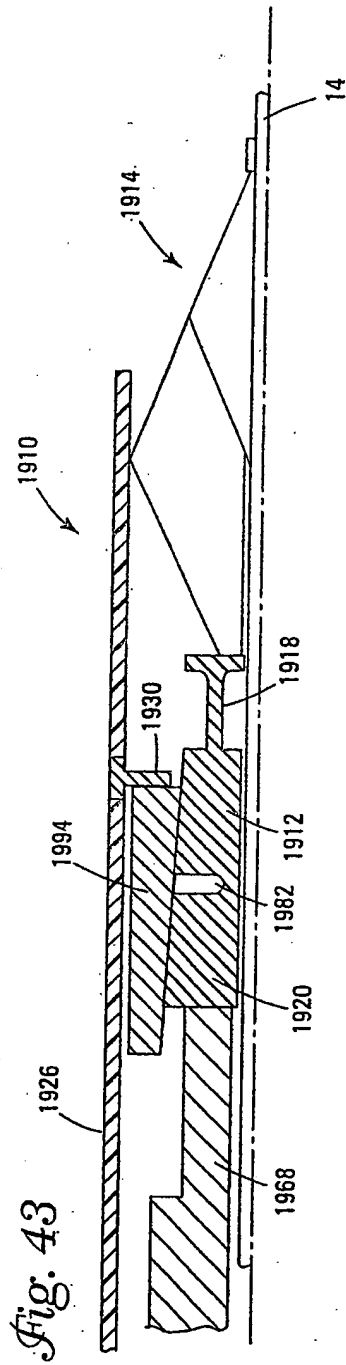
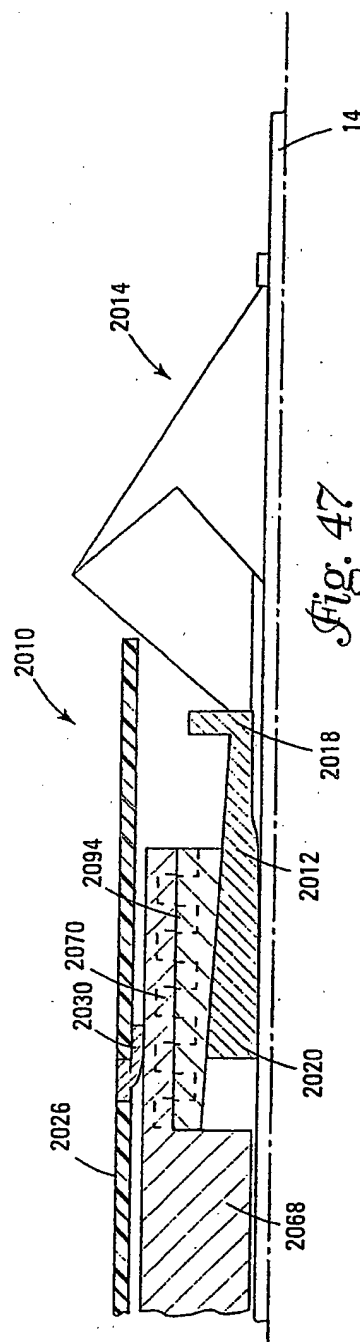
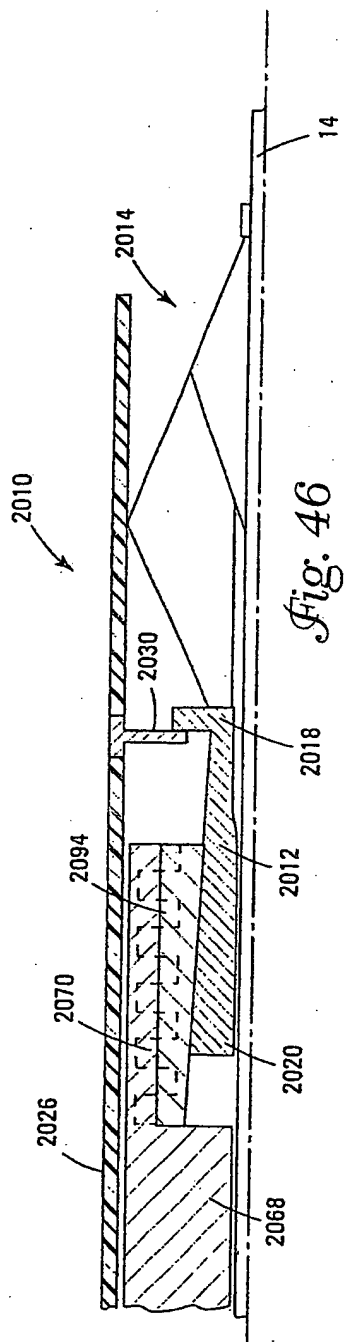


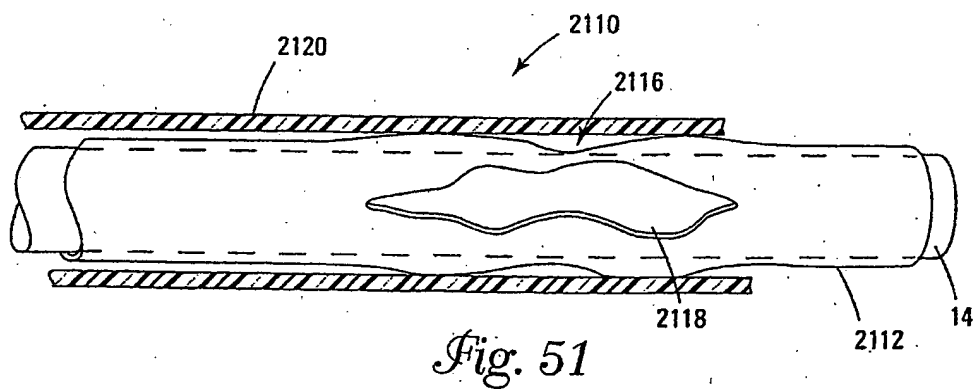
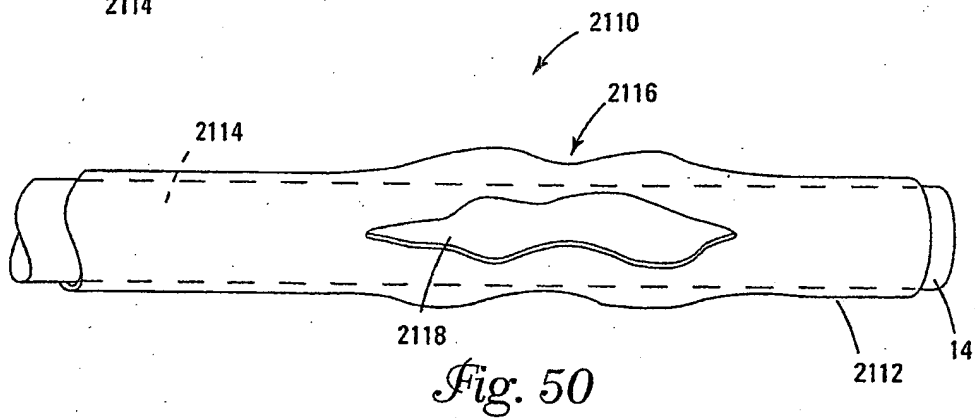
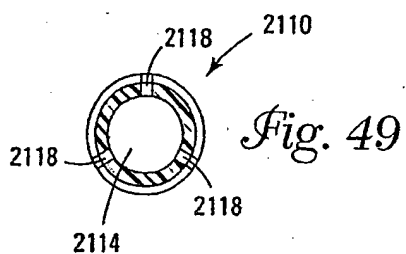
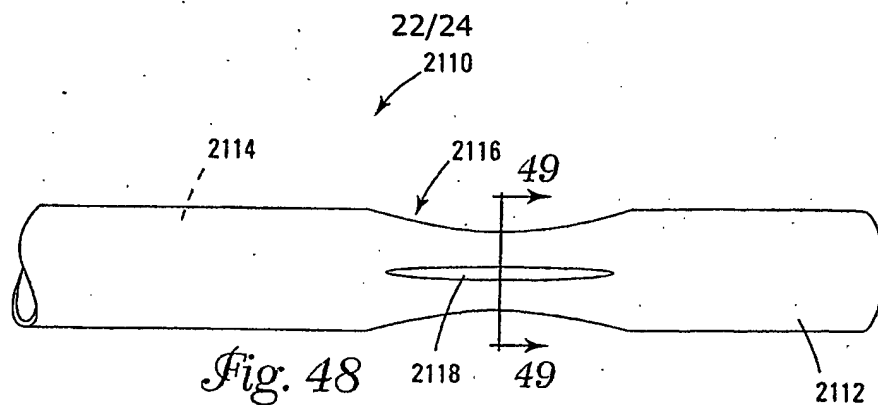
Fig. 40

19/24

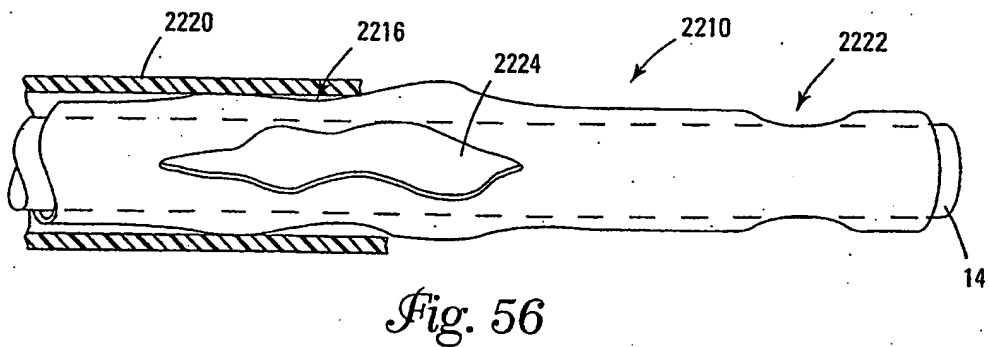
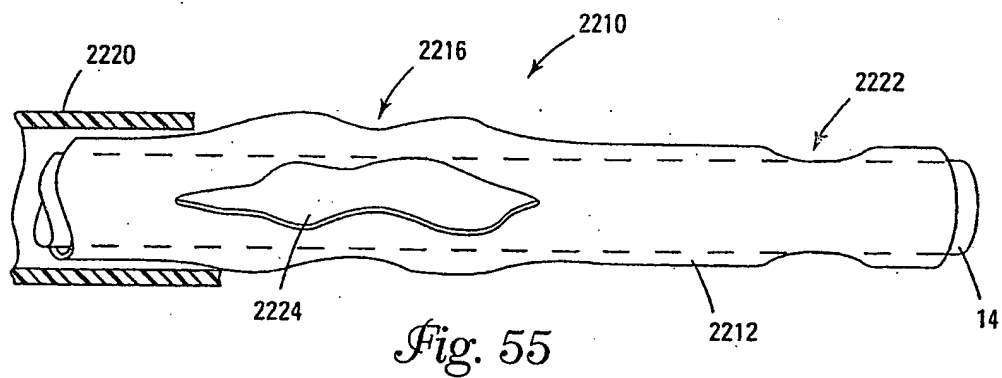
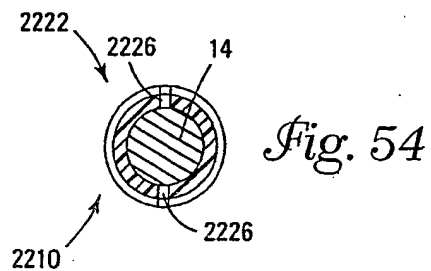
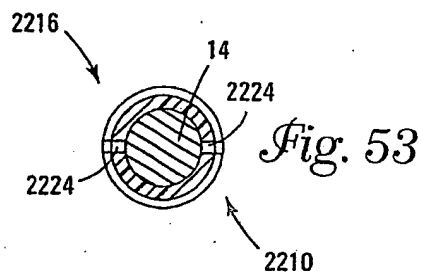
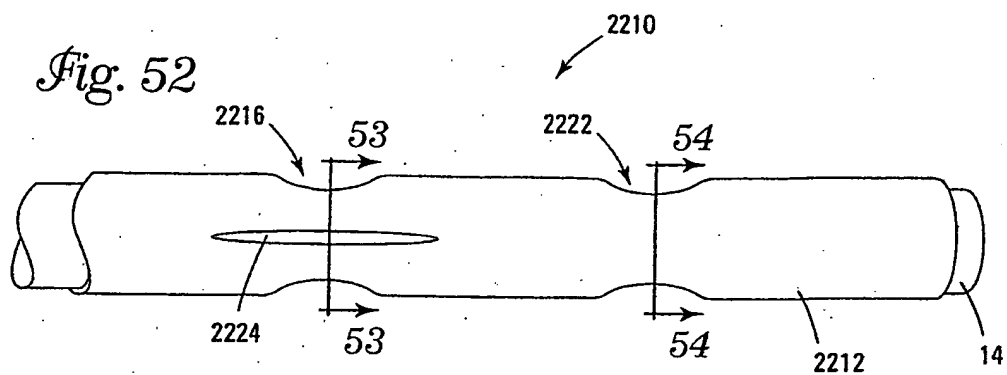








23/24



24/24

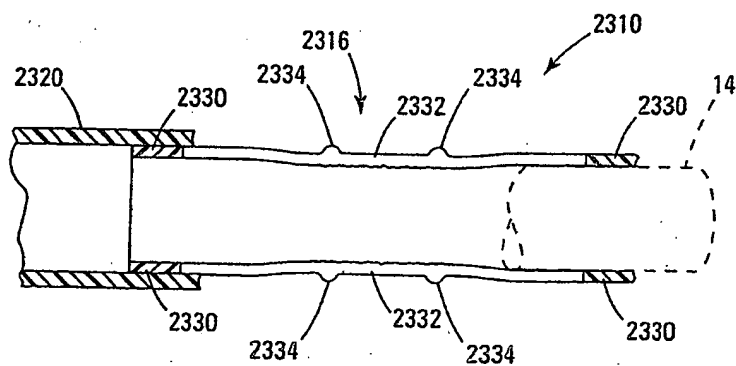
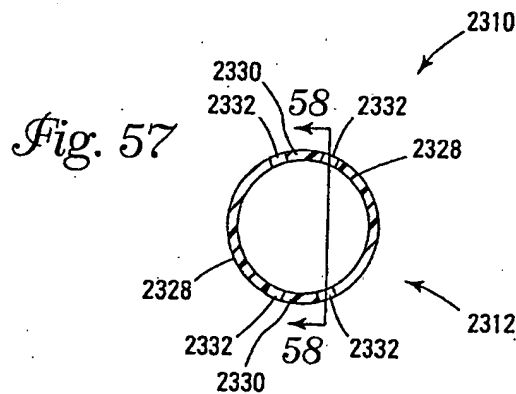


Fig. 58

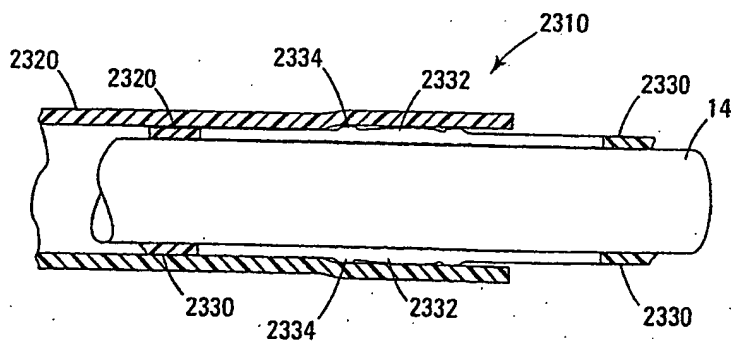


Fig. 59

INTERNATIONAL SEARCH REPORT

International Application No.
PCT/US2004/004096

A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 A61F2/01

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the International search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2002/095174 A1 (CHANG JEAN ET AL) 18 July 2002 (2002-07-18) paragraph '0084! paragraph '0088! figures 12A-12E figures 13A-13C figures 14A,14B	1-34
P, X	WO 2004/012628 A (OFIR GIL ; ROSENSCHEIN URI (IL)) 12 February 2004 (2004-02-12) abstract figures 10A,10B	1-34
A	US 2002/128678 A1 (PETERSEN SCOTT R) 12 September 2002 (2002-09-12) paragraph '0006! figures 1-3	1-34

☐ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents:

- *A* document defining the general state of the art which is not considered to be of particular relevance
- *E* earlier document but published on or after the international filing date
- *L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- *O* document referring to an oral disclosure, use, exhibition or other means
- *P* document published prior to the international filing date but later than the priority date claimed

- *T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- *X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- *Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
- *Z* document member of the same patent family

Date of the actual completion of the international search

24 June 2004

Date of mailing of the international search report

06/07/2004

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentkan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
Fax: (+31-70) 340-3016

Authorized officer

Franz, V

INTERNATIONAL SEARCH REPORT

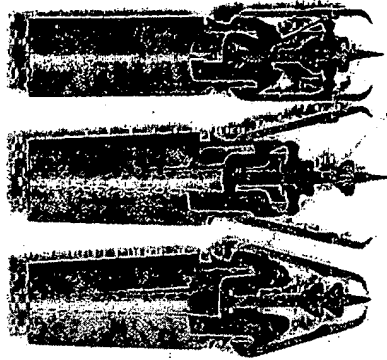
Information on patent family members

International Application No

PCT/US2004/004096

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2002095174 A1	18-07-2002	US 6371971 B1	16-04-2002
		US 2002183782 A1	05-12-2002
		CA 2358706 A1	25-05-2001
		DE 20022465 U1	25-10-2001
		EP 1139912 A1	10-10-2001
		JP 2003513745 T	15-04-2003
		WO 0135857 A1	25-05-2001
WO 2004012628 A	12-02-2004	WO 2004012628 A1	12-02-2004
US 2002128678 A1	12-09-2002	CA 2439826 A1	12-09-2002
		EP 1365703 A2	03-12-2003
		WO 02069844 A2	12-09-2002
		US 2003176887 A1	18-09-2003

A simple, trigger activated stapler deploys the staple extraluminally onto the target vessel.



As the device is activated, the staple expands to maximize the amount of adventitia and media to be approximated.

Case closed.

The Expanding Vascular Staple is just one of the components that make up the innovatively designed EVS™ system.



Delivery sheath enhances vascular access management. The sheath gently locks on to the vessel and maintains control of the puncture site.



The stapler is introduced into the sheath, which protects the soft tissue and the staple.



Immediate re-access of vessel site proximity.



A single operator interacts with the ergonomically designed device.

Close your cases.

angioLINK

Info@angiolink.com
Toll Free: 866-368-1406